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(54) **SYSTEMS AND METHODS FOR ENABLING HEART VALVE REPLACEMENT**

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**A61F 2/24** (2006.01)

(52) **U.S. Cl.**  
USPC ..... **623/2.11**

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USPC ..... 623/1.24, 1.26, 2.1, 2.11, 2.17, 2.38  
See application file for complete search history.

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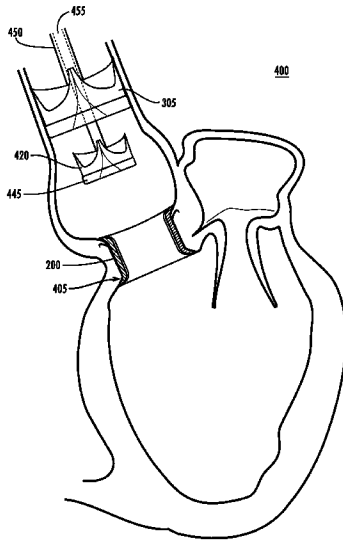
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(57) **ABSTRACT**

The present invention describes a cardiac prosthetic system (400) comprising: an anchoring conduit (200) having a harbor (415), the harbor including a first releasably engaging component (515); a temporary valve (305) and a heart valve prosthesis (420) having a second releasably engaging component (445) enabled to be securely coupled and uncoupled from the first releasably engaging component (515) of the harbor (415).

**42 Claims, 10 Drawing Sheets**



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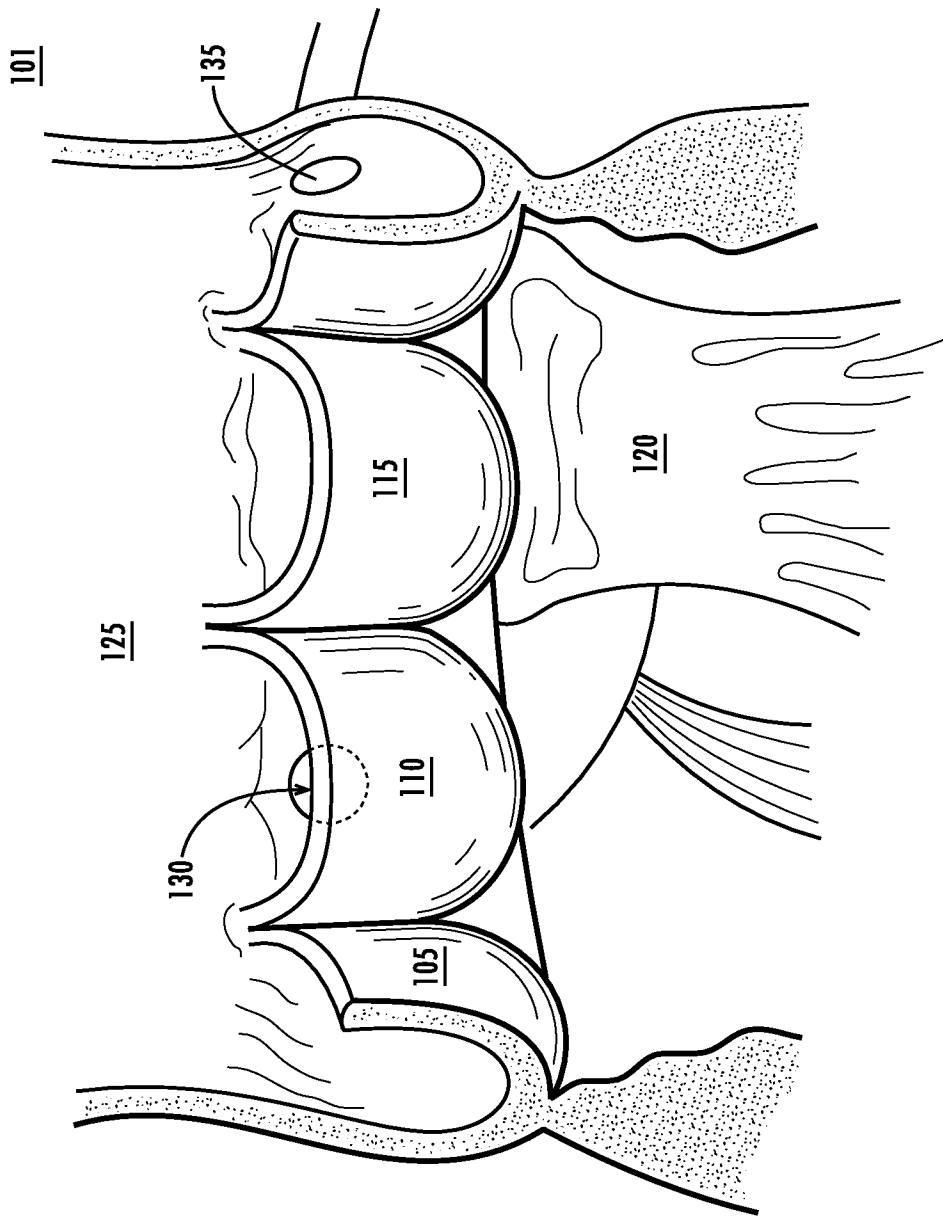
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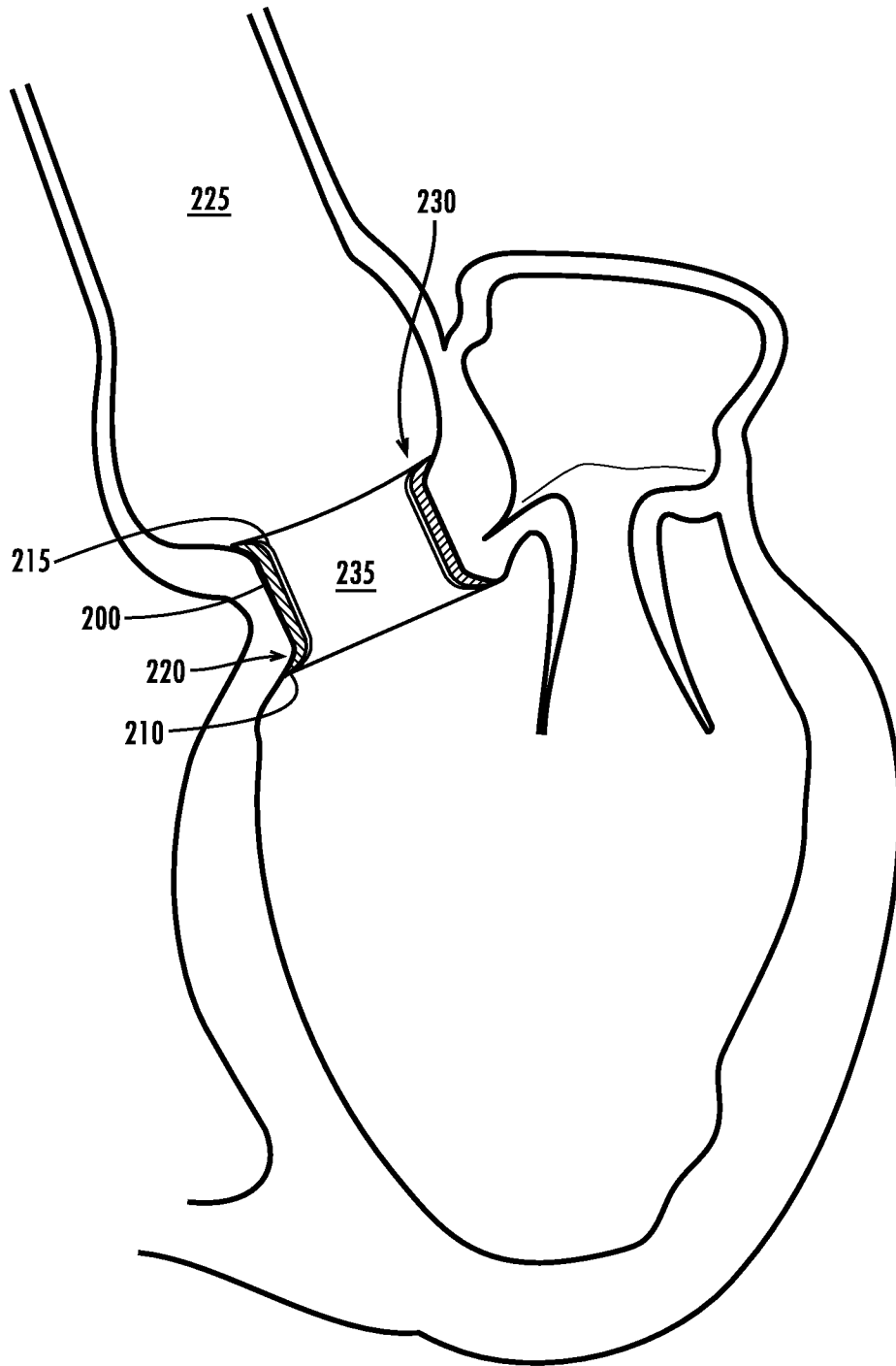
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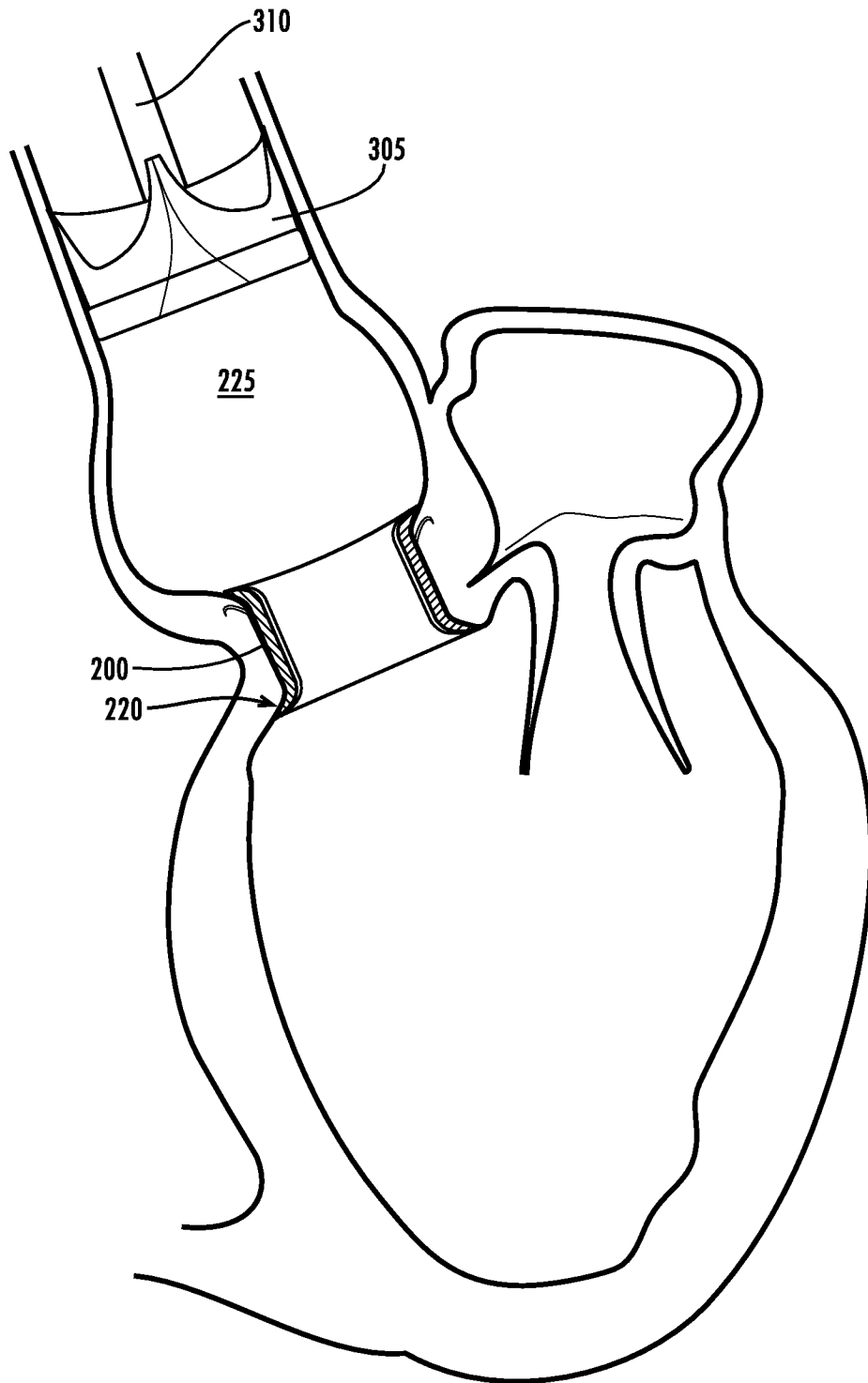
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**FIG. 1**

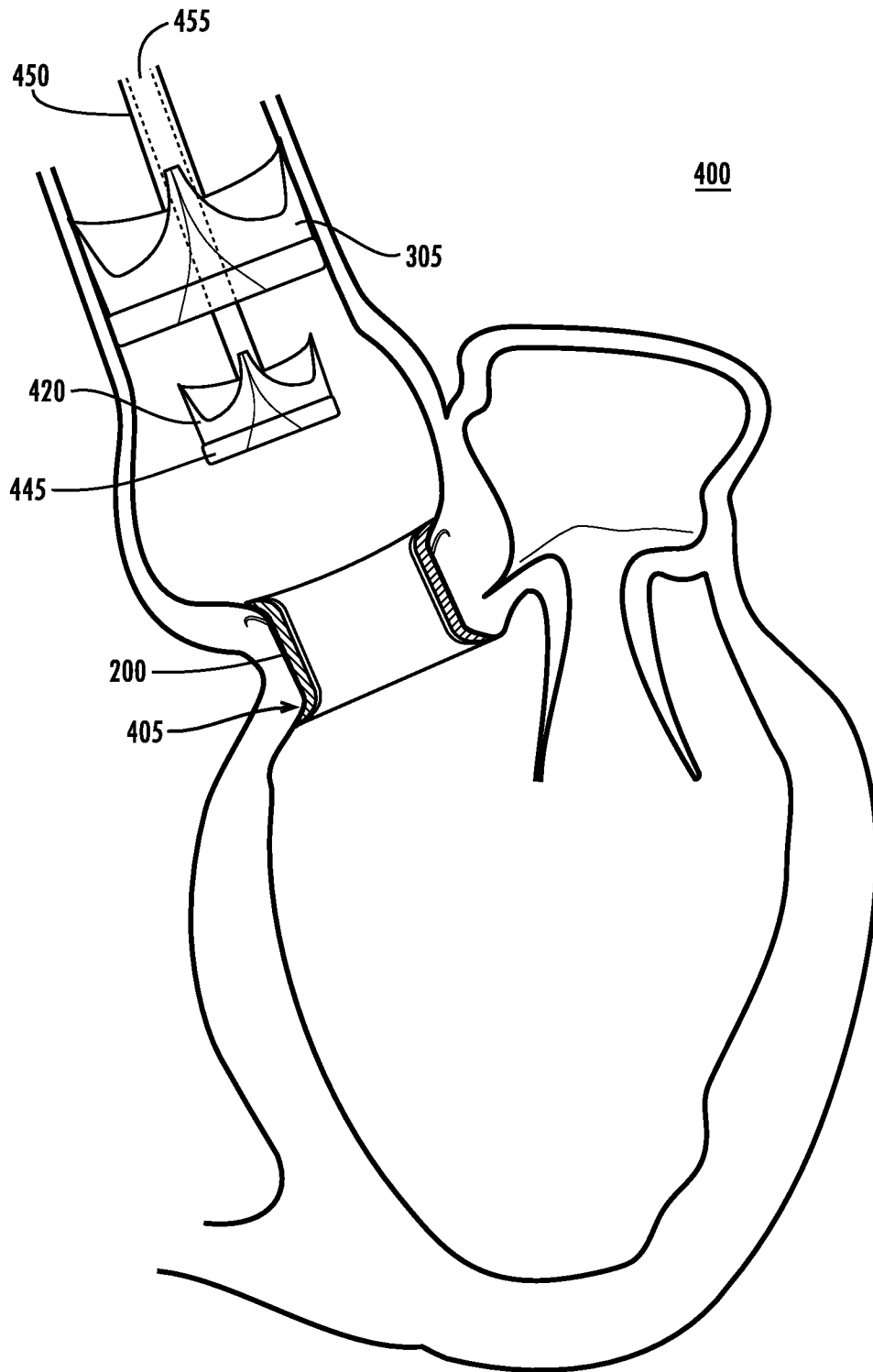


**FIG. 2**

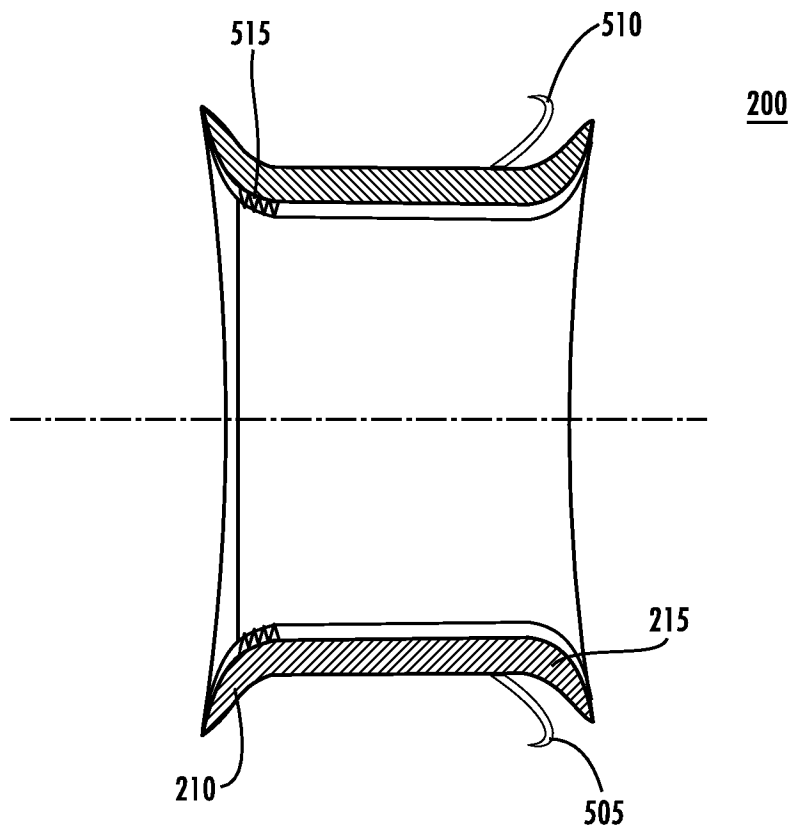


**FIG. 3**





**FIG. 4B**



**FIG. 5A**

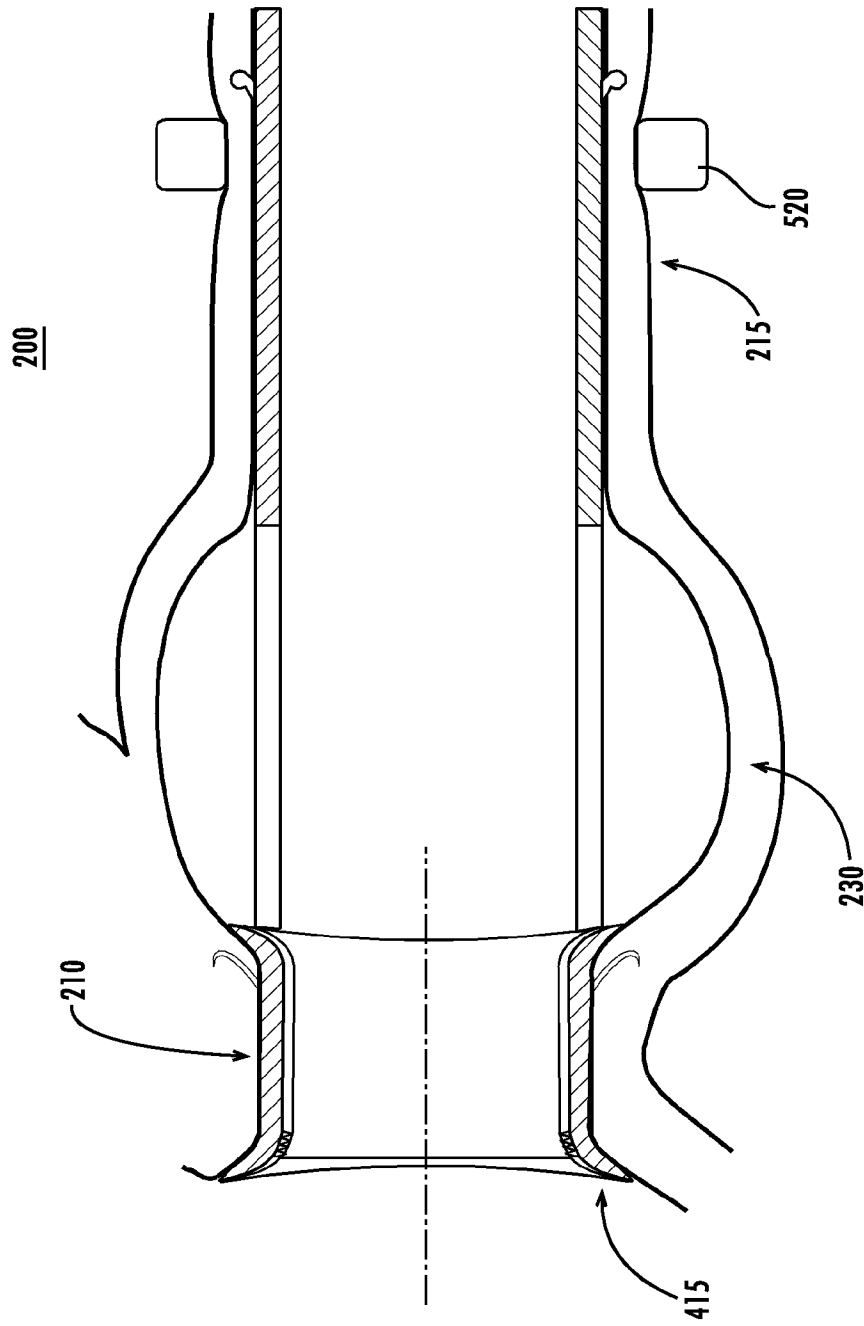


FIG. 5B

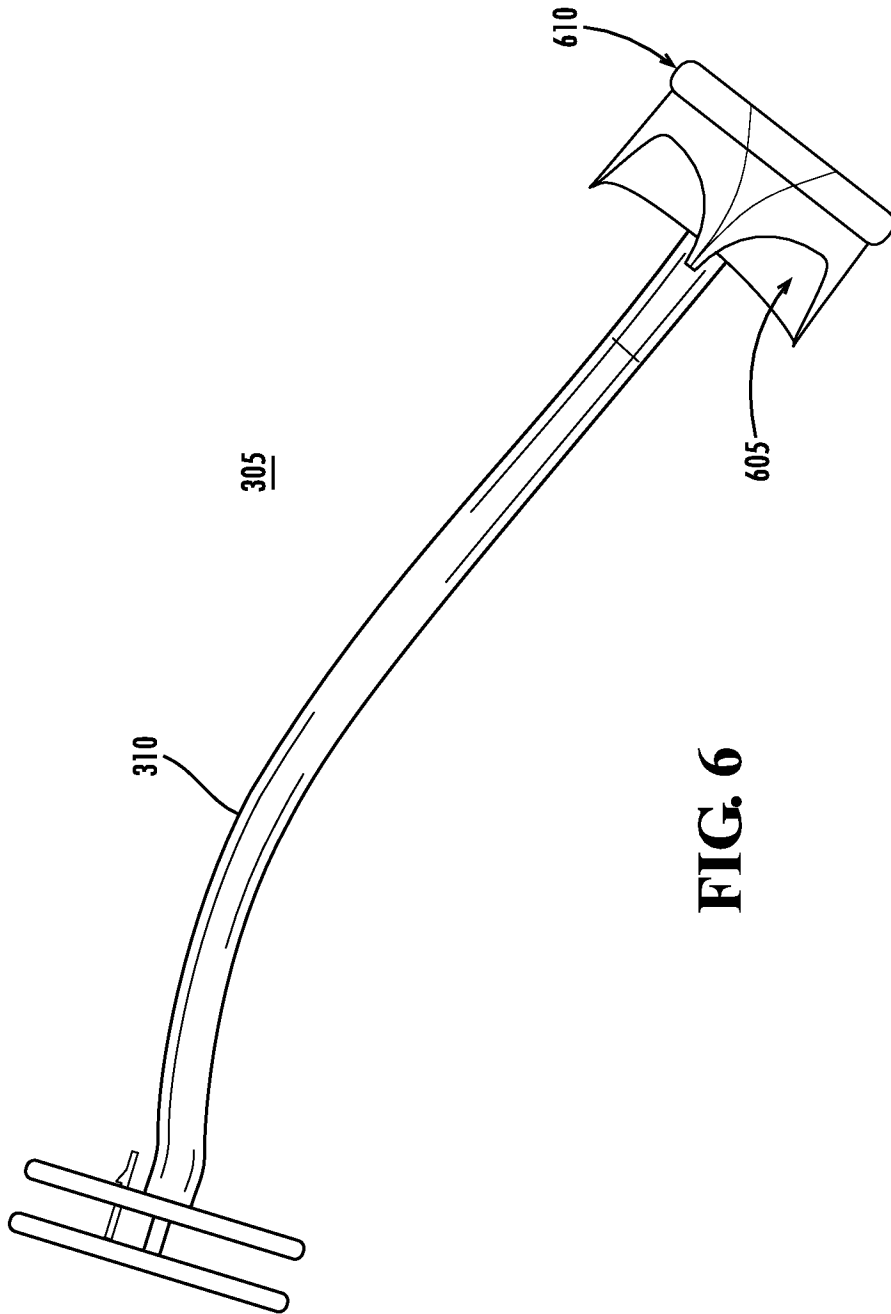
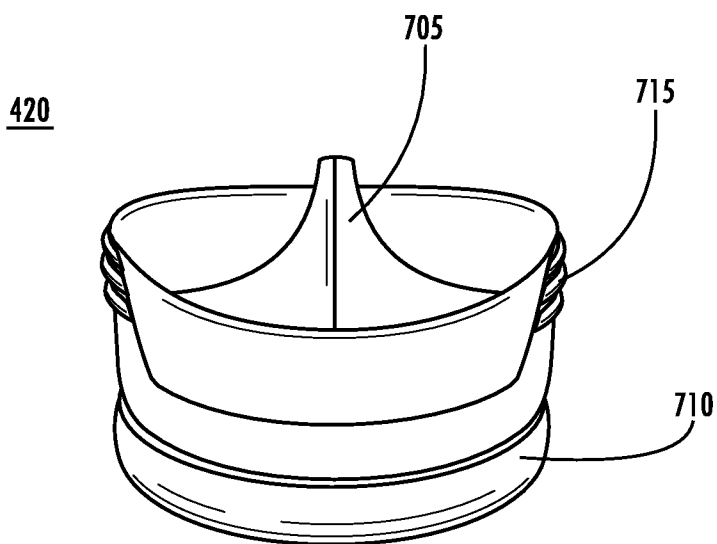
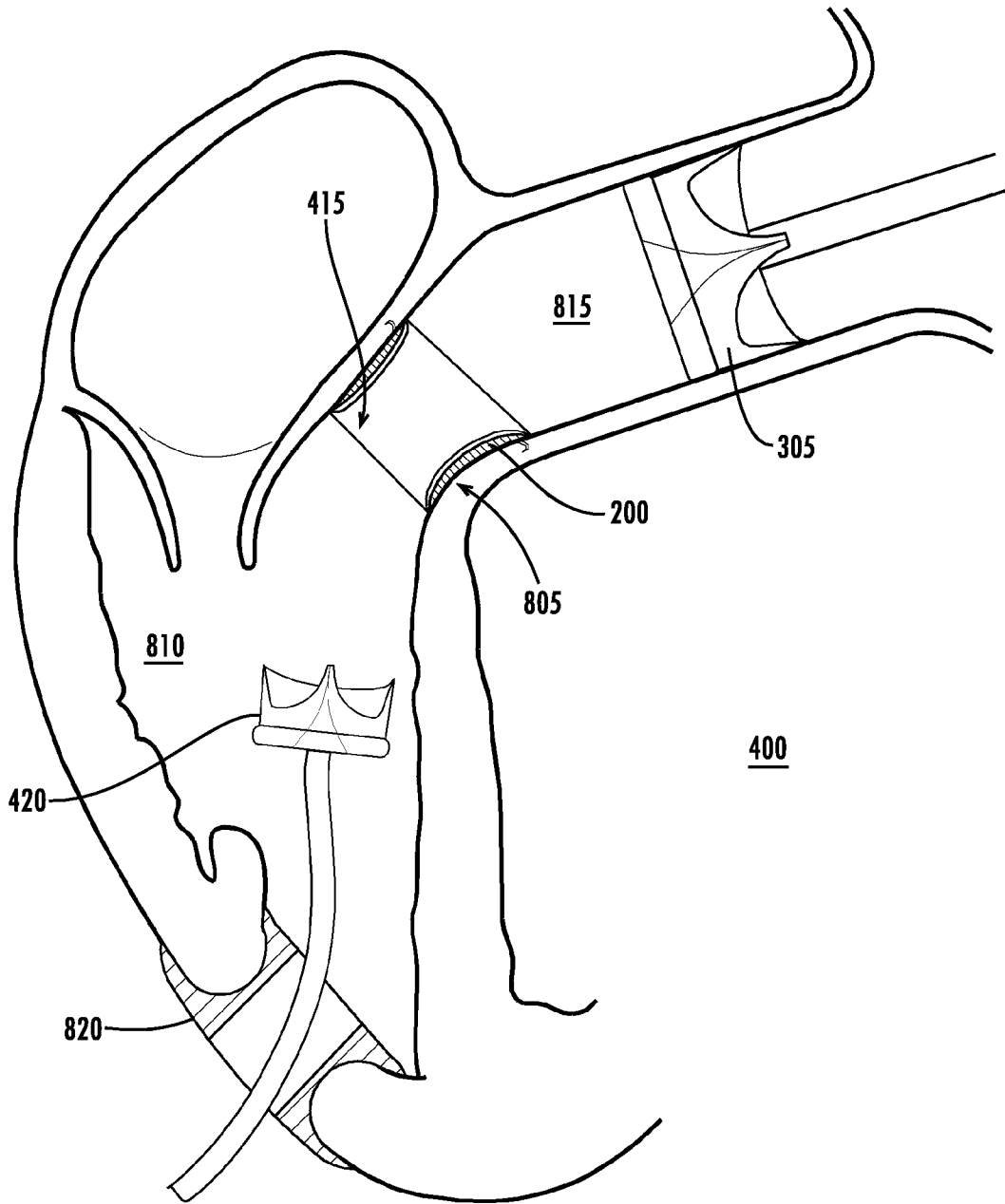


FIG. 6



**FIG. 7**



**FIG. 8**

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## SYSTEMS AND METHODS FOR ENABLING HEART VALVE REPLACEMENT

### BENEFIT AND PRIORITY CLAIMS

This application is a 35 U.S.C. §371 U.S. National Stage of International Application No. PCT/US2006/062199 filed 15 Dec. 2006, which claims priority to and the benefit of U.S. Ser. No. 60/750,558, filed 15 Dec. 2005. All of said prior applications are hereby incorporated by reference in their entirety as if fully set forth below.

### CROSS REFERENCE TO RELATED APPLICATIONS

This application claims the benefit of U.S. Provisional Application No. 60/750,558, filed 15 Dec. 2005, which is hereby incorporated by reference in its entirety as if fully set forth below.

### FIELD OF THE INVENTION

This invention refers generally to the field of heart valve replacement, and specifically to the implants tools and methods for preparing a native heart valve for a prosthesis and for providing a replaceable heart valve prosthesis.

### BACKGROUND OF THE INVENTION

Cardiovascular disease accounts for nearly fifty percent of deaths in both the developed world and in developing countries. Indeed, the risk of dying from heart disease is greater than the risk from AIDS and all forms of cancer combined. Cardiovascular disease causes 12 million deaths in the world each year. It is the leading cause of death in the U.S., killing some 950,000 people each year. It also accounts for a significant amount of disability and diminished quality of life. Some 60 million people in the U.S. alone have some form of heart disease. Therefore, a great need exists for the advancement of devices and procedures to cure, treat, and correct a wide variety of forms of heart disease.

Normal heart function primarily relies upon the proper function of each of the four valves of the heart, which pass blood through the four chambers of the heart. The four chambers of the heart include the right atrium and left atrium, the upper chambers, and the right ventricle and left ventricle, the lower chambers. The four valves, controlling blood flow in the chambers, include the tricuspid, mitral, pulmonary, and aortic valves. Heart valves are complex structures that rely on the interaction of many components to open and close the valve. More particularly, each of the four valves of the heart have leaflets, comprised of fibrous tissue, which attach to the walls of the heart and aid in controlling the flow of blood through the valve. The mitral valve has two leaflets and the tricuspid valve has three leaflets. The aortic and pulmonary valves have three leaflets that are more aptly termed "cusps," stemming from their half moon shape.

The cardiac cycle involves the pumping and distribution of both oxygenated and deoxygenated blood within the four chambers. In systole, or the rhythmic contraction of the heart cycle, blood that has been oxygenated by the lungs enters the heart into the left atrium. During diastole, or the resting phase of heart cycle, the left atrial pressure exceeds the left ventricle pressure; thus, oxygenated blood flows through the mitral valve, a one way inflow valve, into the left ventricle. The contraction of the left ventricle in systole pumps the oxygenated blood through the aortic valve, into the aorta, and is

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passed to the body. When the left ventricle contracts in systole, the mitral valve closes and the oxygenated blood passes into the aorta rather than back through the mitral valve. On the other side of the heart, deoxygenated blood returns from the body and enters the heart through the right atrium. This deoxygenated blood flows through the tricuspid valve into the right ventricle. When the right ventricle contracts, the tricuspid valve closes and the deoxygenated blood is pumped through the pulmonary valve. Deoxygenated blood is directed to the pulmonary vascular bed for oxygenation, and the cardiac cycle repeats itself.

The performance of the cardiac cycle by the various components of the heart is a complex and intricate process. Deficiency in one of the components of the heart or deficiency in the performance of the cardiac cycle most often leads to one or more of the numerous different types of heart disease. One prevalent heart disease condition is aortic valve regurgitation. Aortic valve regurgitation has many levels of severity. Aortic regurgitation is the diastolic flow of blood from the aorta into the left ventricle. Regurgitation is due to incompetence of the aortic valve or disturbance of the valvular apparatus (e.g., leaflets, annulus of the aorta) resulting in diastolic flow of blood into the left ventricular chamber. Incompetent closure of the aortic valve can result from intrinsic disease of the cusp, diseases of the aorta, or trauma. Aortic regurgitation may be a chronic disease process or it may occur acutely, presenting as heart failure. Diastolic reflux through the aortic valve can lead to left ventricular volume overload.

FIG. 1 provides an illustration of a normal aortic valve **101**. The perspective of the aortic valve **101** shown in FIG. 1 provides a diagram of a dissected and flattened aortic valve **101** to best illustrate its components. The aortic valve **101** has three cusps or leaflets, the left coronary cusp **105**, the right coronary cusp **110**, and the non-coronary cusp **115**. These three cusps control the flow of blood from the left ventricle into the aorta, which ultimately conveys oxygenated blood to the tissues of the body for their nutrition. Located just above the three cusps, **105**, **110**, and **115**, are the sinuses of the aorta and each sinus corresponds to each individual cusp. The origins of the coronary arteries are proximate the sinuses of the aorta **125**. As shown in FIG. 1, the orifice **130** for the right coronary artery is located just above the right coronary leaflet cusp **110**. Similarly, the orifice **135** for the left coronary artery is located just above the left coronary leaflet cusp **105**. Additionally, the aortic valve **101** is juxtaposed with the anterior mitral annulus **120**.

In a normal aortic valve **101**, when the left ventricle contracts in systole, the aortic valve cusps, **105**, **110**, and **115**, open into the aorta and blood flows from the left ventricle into the aorta. When the left ventricle rests in diastole, the cusps, **105**, **110**, and **115**, meet and close, covering the area of the valve annulus. Therefore, the cusps, **105**, **110**, and **115**, prevent regurgitation, or backflow of blood, into the left ventricle during diastole.

The aortic valve **101** is located in the aortic root of the aorta. The aortic root has two main components, the inner (aorto-ventricular junction) and the outer (sino-tubular junction), which are considered the functional aortic annulus. It is this aortic annulus that supports the fibrous structures of the cusps, **105**, **110**, and **115**.

As shown in FIG. 1, the function of the aortic valve, involves the complex interaction of numerous components. If one of the components or functions of the complicated interaction fails, then aortic valve regurgitation can result. For example, a bicuspid valve, calcification of the cusps, or stenosis or restricted motion of the cusps can lead to aortic regurgitation. Prolonged and/or severe aortic valve regurgitation

can lead to compensatory left ventricle dilation. Aortic valve regurgitation is a progressive condition that, if not corrected, can be fatal.

In addition to aortic regurgitation, pulmonic regurgitation is highly prevalent heart disease that causes or contributes to increasing numbers of heart disease each year. Like aortic regurgitation, pulmonic regurgitation involves the incompetence of the pulmonic valve and its failure to completely close. In a normal pulmonic valve, the right ventricle contracts in systole and pumps blood through the open pulmonic valve into the pulmonary artery. Contrastingly, when the right ventricle rests in diastole, the pulmonic valve closes and prevents the backflow of blood into the right ventricle. In cases of pulmonic regurgitation, the pulmonic valve fails to completely close and permits a regurgitant flow of blood from the pulmonary artery back into the right ventricle during diastole. This backflow of blood can overload the right ventricle and lead to right ventricle dilation.

There a large variety of methods available in the prior art to treat different types of valvular heart disease such as pulmonic regurgitation and aortic regurgitation. A highly popular and successful method of treatment of these conditions involves the use of prosthetic cardiac valves, such as mechanical valves and bioprosthetic valves.

The most commonly used replacement devices are mechanical and bioprosthetic valves, with homografts and autografts less commonly used. From 1990 to 2000, the breakdown of valve replacement percentages as indicated by the Society of Thoracic Surgery Registry for patients less than 60 years of age with aortic valve disease was as follows: mechanical valves in 77% of patients, bioprosthetic valves in 13%, homograft valves in 5%, and the Ross procedure in 5%.

A mechanical valve is a device constructed from man-made materials and is used to replace patients damaged or diseased native heart valves. More than 60 percent of heart valve replacements have been made with mechanical prostheses due to their durability and superior hemodynamics which offer minimal resistance to flow. Despite their superior durability, the turbulent fluid mechanics of mechanical valves causes damage to blood cells. This damage to the blood cells can include thrombus formation. The possible thrombus formation initiated by disturbed flow patterns necessitates lifelong anticoagulant therapy. Further problems are associated with mechanical heart valves, including small stagnant regions proximate the hinges that sometimes lead to bacterial infections causing further heart damage.

Many different valve designs with different materials of construction have evolved to address the deficiencies of mechanical valves, such as to reduce thrombus formation and decrease the mechanical stresses that can cause blood cell damage. Several synthetic polymers have been tested as leaflet materials such as silicone, polyolefin rubbers and polytetrafluoroethylene. Laboratory fatigue testing has illustrated that polyurethane valves are capable of achieving more than 800 million cycles (~20 years of "normal" function). Valve leaflets constructed of a commercially available polyetherurethane when implanted in sheep showed superior valve function to that of bioprosthetic valves. Thus, polymeric valves could offer a clinical advantage with the promise of improved durability compared to bioprostheses and low thrombogenicity compared to mechanical valves. Although polymeric valves show great promise they have been under development for several decades and no design has made it to commercialization due to failure or calcification within its normal biological environment. As a result, mechanical valves are still the primary choice for surgical correction and have to be used

in conjunction with anticoagulation therapies, which reduces the quality of life of the patient and exposes them to risks associated with bleeding.

Bioprosthetic valves are tissue valves made of animal tissue (i.e. xenografts) and are easily and readily available. These were introduced in the early 1970s as an attempt to avoid some of the disadvantages of mechanical valves. Flexible, trileaflet, biological tissue valves mimic their natural counterparts more closely than mechanical heart valves. Their central flow characteristics offer better hemodynamic efficiency, and their biological surfaces enhance thromboresistance as compared to mechanical prostheses.

The valves are chemically treated to make the tissue less immunogenic and thus less likely to incite an allergic or immunological reaction in the recipient. As a result, the tissue comprising the valve is non-viable, and therefore, subject to degeneration with time. Bioprosthetic valves are commonly employed in elderly patients for whom the risk of bleeding complications are high and in those whose desired way of life precludes the discipline of anticoagulation therapy.

The biological tissues are usually fixed with different chemicals (glutaraldehyde, Aminooleic acid, ethanol etc) and under different protocols in order to increase the durability of the valve. Leaflet fixation stiffens the tissue unintentionally, alters internal shear properties, increases shear stiffness, stress relaxation and hysteresis, and causes substantial dehydration, all of which lead to valve failure due to calcification or tissue tearing. Although some chemical treatments are effective in reducing calcification, they do not prevent disruption of collagen fibers. Collagen fibers exposed to blood flow are damaged and cannot be repaired due to lack of viable cells within the leaflet. Therefore because of tissue degradation and calcification bioprosthetic valves have a limited durability which may average around 10 years. Although bioprosthetic valve technology has advanced, their limited durability is a problem which may take a long time to address completely.

Currently a new generation of bioprosthetic valves and mechanical valves is being developed, and these valves may be implanted percutaneously. While these bioprosthetic and mechanical valves present a number of improvements over the prior art, the safety and success of these devices is significantly reduced by the complexity of their deployment.

Many devices exist in the prior art, which attempt to address the complexity of properly deploying a bioprosthetic valve. For example, U.S. Pat. No. 6,790,230 to Beyersdorf et al. ("230 patent") discloses a conventional valve anchoring element, which has non-cylindrical form that corresponds to the shape of the aorta. The anchoring element of the '230 patent is provided such that a replacement valve can be sutured to the interior of the anchoring element. The anchoring element and associated replacement valve can then be delivered via a catheter to the aorta and expanded such as to disable the native aortic valve. Thereby, the expansion of the anchoring element in the aorta serves to disable the native aortic valve and, at the same time, enable the replacement valve.

U.S. Pat. No. 7,018,406 to Seguin et al. ("406 patent") discloses a prosthetic valve assembly to be used in replacing a deficient native valve. The prosthesis described in the '406 patent includes a tissue valve supported on a self expandable stent. The prosthesis is capable of percutaneous delivery to the native valve, at which the prosthesis can be expanded and attached to the lumen wall. The '406 patent describes that the typical valve is made biological materials and is attached to the valve support band with a suture. The valve attached to the

valve support band is collapsible along its center axis so that the entire structure can be compressed and loaded onto a catheter for delivery.

U.S. Patent Publication No. 2005/0137689 to Salahieh et al. ("689 Publication") discloses a method for endovascularly replacing a heart valve. The method disclosed in the '689 Publication includes the steps of delivering a replacement valve and an expandable anchor in an unexpanded configuration within a catheter to a vicinity of a heart valve. Once delivered to the proper location, the anchor is deployed from the catheter and expanded to contact tissue at an anchor site. The expansion of the anchor simultaneously deploys the collapsed replacement heart valve contained within the anchor.

The deployment of these conventional bioprosthetic valves requires the precise execution of a number of steps and techniques, and inaccurate execution of even one of these steps can lead to a patient fatality. For example, proper deployment of the bioprosthetic valve can require expansion of the valve anchor at a precise location within the native heart valve. Furthermore, the valve anchor must properly engage the lumen wall when expanded such that a good surface of contact is made with the lumen wall to enable a tight contact. Good and safe seating of the valve anchor is critical, as it must withstand blood flow under high pressure, high velocity, and a significant amount of pulsation. Furthermore, a replacement valve positioned in an inadequately anchored valve will not be able to resist the forces of the constantly changing vessel wall diameter and turbulent blood flow. Improper and insufficient deployment can lead to migration of the valve anchor before or after the deployment of the bioprosthetic valve. Even the slightest migration of the valve anchor can have many detrimental results, including covering the openings to an arterial outlet or compromising the function of the replacement valve.

Not only is precise placement of the valve anchor of a bioprosthetic valve important, a secure seating of the valve anchor is critical because improper or insufficient deployment of the valve anchor can lead to leakage between the anchor and the lumen wall. It is often the case that a deficient native valve and areas of tissue around the native valve have irregularities and calcification that are a result of, or are contributing factors to, the heart disease at issue. The typical calcification, thickening, and hardening of the cardiac annulus can make it increasingly difficult to achieve proper sealing quality for the valve anchor of the bioprosthetic valve. For example, heavy calcification on the native valve can lead to bumpy and even surfaces, which can translate to a low quality seal of the valve anchor with the lumen wall if not deployed properly. Not only can calcification make it difficult to properly seat the valve anchor, fragments of the calcified deposits can be loosened during the seating of the valve anchor and thus enter blood stream causing damage and possible blockage.

While many of the conventional devices have attempted to address the issues and complexities associated with the minimally invasive deployment of a heart valve replacement, significant problems and risks for the patient still exist. A large majority of the risk is due to the nature of the deployment of the replacement valves. Often, a surgeon has one shot to correctly deploy the heart valve prosthesis. Furthermore, the endovascular deployment of the heart valve provides a surgeon with a limited ability to verify the correctness and accuracy of the deployment. The surgeon's deployment of the replacement valve is often visually aided only by a two dimensional ultrasound image. This two dimensional image leaves a large amount of room for error in the three dimensional deployment of the replacement valve. For example, the

valve anchor could appear properly seated on the ultrasound image, but the side of the valve anchor not visible in the image could be misaligned and/or improperly sealed with the lumen wall. As described, a slightly improper seal or slight misplacement of the valve anchor can lead to catastrophic and even fatal results. Additionally, once the replacement valve has been fully deployed, it is difficult or impossible to change the position of the prosthesis without damaging the native structure.

As a result of the limitations of both bioprosthetic heart valve and mechanical valves, patients have to choose between quality of life and durability of the repair. Additionally there is a group of patients which may not tolerate the risks associated with a mechanical valve, but may limit their lives using a bioprosthetic valve as a second operation to replace this valve can be considered clinically not viable.

Therefore, it would be advantageous to provide an apparatus and method to prepare a deficient native valve for replacement.

Additionally, it would be advantageous to provide an apparatus and method for accurate and efficacious deployment of a valve anchor.

Additionally, it would be advantageous to provide an apparatus and method for accurate and efficacious deployment of a valve anchor independent of a replacement heart valve.

Additionally, it would be advantageous to provide an apparatus and method for correcting valvular heart disease that allows for accurate and efficacious deployment of a heart valve prosthesis.

Additionally, it would be advantageous to provide an apparatus and method for correcting valvular heart disease that allows for viable methods to conduct repeat operations on a heart valve.

Additionally, it would be advantageous to provide an apparatus and method for correcting valvular heart disease that allows for viable methods to replace a previously deployed heart valve prosthesis.

Additionally, it would be advantageous to provide an apparatus and method for correcting valvular heart disease that allows for deployment of a replaceable heart valve prosthesis implemented in a minimally invasive manner.

Additionally, it would be advantageous to provide a releasably connected heart valve prosthesis delivered with a long arm or steerable needle from outside the heart to a valve of a beating heart.

Additionally, it would be advantageous to provide a smooth and substantially uniform surface within a lumen for deployment of a heart valve prosthesis.

Additionally, it would be advantageous to provide a backup system capable of permitting a patient to go on bypass if a heart valve replacement procedure fails.

Additionally, it would be advantageous to provide an apparatus capable of providing a separately deployable harbor for releasably connecting a heart valve prostheses.

## BRIEF SUMMARY OF THE INVENTION

The present invention describes methods and apparatus to prepare a heart valve for replacement and improve a deficient heart valve. An exemplary embodiment of the method of preparing a heart valve for replacement involves delivering an anchoring conduit to a heart valve. The anchoring conduit is expanded in the heart valve and the expansion of the anchoring conduit disables the heart valve. Furthermore, the expansion of the anchoring conduit defines an open cavity.

An exemplary embodiment of the method of improving a deficient heart valve involves delivering an anchoring conduit

to a heart valve. The anchoring conduit has a harbor, which is enabled to releasably connect a heart valve prosthesis. Then, a temporary valve is delivered in a condensed state to a target site in an artery proximate the heart valve. Subsequently, the anchoring conduit is deployed in the heart valve, disabling the heart valve. The temporary valve operates to temporarily replace the function of the heart valve when the anchoring conduit is expanded.

These and other objects, features and advantages of the present invention will become more apparent upon reading the following specification in conjunction with the accompanying drawing figures.

#### BRIEF DESCRIPTION OF THE FIGURES

FIG. 1 provides an illustration of a normal aortic valve 101.

FIG. 2 provides an illustration of an exemplary embodiment of an anchoring conduit 200 implemented in aortic valve in accordance with an exemplary embodiment of the present invention.

FIG. 3 provides an illustration of an exemplary embodiment of anchoring conduit 200 and temporary valve 305 implemented in an aortic valve in accordance with an exemplary embodiment of the present invention.

FIG. 4A provides an illustration of an exemplary embodiment of a cardiac prosthetic system 400 implemented in aortic valve in accordance with an exemplary embodiment of the present invention.

FIG. 4B provides an illustration of an alternative embodiment of a cardiac prosthetic system 400 implemented in aortic valve in accordance with an exemplary embodiment of the present invention.

FIG. 5A provides an illustration of an exemplary embodiment of an anchoring conduit 200 in accordance with an exemplary embodiment of the present invention.

FIG. 5B provides an illustration of an exemplary embodiment of an anchoring conduit 200 in accordance with an exemplary embodiment of the present invention.

FIG. 6 provides an illustration of an exemplary embodiment of a temporary valve 305 in accordance with an exemplary embodiment of the present invention.

FIG. 7 provides an illustration of an exemplary embodiment of a heart valve prosthesis 420 in accordance with an exemplary embodiment of the present invention.

FIG. 8 provides an illustration of an exemplary embodiment of a cardiac prosthetic system 400 implemented in a pulmonic valve in accordance with an exemplary embodiment of the present invention.

#### DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

The present invention addresses the deficiencies in the prior art by providing a minimally invasive apparatus and method for preparing a heart valve for replacement and for deploying a replaceable heart valve prosthesis. The apparatus and method of preparing a heart valve for replacement can be used to improve the success and efficacy of heart valve repair. The medical device and method of improving a deficient heart valve disclosed herein can be used to repeatedly deploy a heart valve prostheses within a deficient valve of the heart. Enabling the efficacious replacement of a heart valve can provide an effective manner of treating valvular heart disease without many of the drawbacks associated with conventional devices and methods. Significantly, the cardiac prosthesis system of the present invention provides a solution which does not force patients to choose between the quality of life

associated with bioprosthetic valves and long term durability associated with mechanical valves. Additionally, this procedure can allow beating heart minimally invasive approaches which can benefit the clinical outcome of heart valve replacements.

An exemplary embodiment of the present invention provides a method of preparing a heart valve for replacement. The method involves the step of delivering an anchoring conduit to a heart valve. Subsequently, the anchoring conduit is expanded in the heart valve. Once the anchoring conduit has been expanded, it defines an open cavity.

In an exemplary embodiment, the open cavity does not contain any leaflets or other elements of a heart valve prosthesis. Furthermore, in an exemplary embodiment, the open cavity has a substantially uniform inner surface. The term substantially uniform is used herein to describe a surface that is generally uniform but may include certain undulations or features. For example, the term substantially uniform surface of the open cavity of the anchoring conduit could describe a cavity that includes a releasably engaging component. Therefore, the substantially uniform surface of the cavity is generally uniform, but not entirely uniform in some embodiments.

The smooth and substantially uniform inner surface of the exemplary embodiment of the expanded form of the anchoring conduit provides a more safe and reliable surface on which to deploy a heart valve prosthesis. Typically, a deficient native valve and the areas of tissue around the native valve have irregularities and heavy calcification. The common calcification, thickening, and hardening of the cardiac annulus can make it increasingly difficult to achieve proper sealing quality for a valve anchor. For example, the existing annulus of the deficient native valve can have a surface that is to varying degrees irregular and calcified, which not only lessens the quality of the support of the anchoring conduit but also acts as a source of leaks between the anchoring conduit and the valve annulus. The exemplary embodiment of the present invention can provide an anchoring conduit to aid in the placement of a heart valve prosthesis and overcome the complexities associated with the irregular and calcified surface of a deficient valve annulus. The smooth and substantially uniform inner surface of the anchoring conduit, as opposed to the bumpy and calcified surface of native valve, can enable a more efficacious and reliable deployment of a replaceable heart valve. An exemplary embodiment of the anchoring conduit is capable of deployment independent of the deployment of the heart valve prosthesis. Furthermore, the quality of the seating of the anchoring conduit can be assessed and verified prior to the introduction of the heart valve prosthesis into the patient's body.

An exemplary embodiment of the present invention also provides a method of improving a deficient heart valve. The method first involves delivering an anchoring conduit to a heart valve. The anchoring conduit has a harbor, which is enabled to releasably connect a heart valve prosthesis. A temporary valve is delivered in a condensed state to a target site in an artery proximate the heart valve. The temporary valve can be expanded at the target site in the artery proximate the heart valve. Subsequently, the anchoring conduit can be expanded in the heart valve and the native components of the heart valve compress against the heart valve and disable the heart valve. The temporary valve can operate to temporarily replace the function of the heart valve when the anchoring conduit is expanded.

Furthermore, the present invention enables a cardiac prosthetic system capable improving a deficient heart valve. In an exemplary embodiment, the deficient heart valve can either be a native valve in the heart or heart valve prosthesis previ-

ously deployed in the heart. An exemplary embodiment of the cardiac prosthetic system in accordance with the present invention provides an anchoring conduit having a harbor. The harbor includes a first releasably engaging component. Furthermore, the cardiac prosthetic system provides a temporary valve. Additionally, a heart valve prosthesis is provided, having a second releasably engaging component enabled to be securely coupled and uncoupled from the first releasably engaging component of the harbor.

FIG. 2 provides an illustration of an exemplary embodiment of an anchoring conduit **200** implemented in an aortic valve in accordance with an exemplary embodiment of the present invention. As shown in FIG. 2, the anchoring conduit provides an expandable structure with a proximal anchor component **210** and a distal anchor component **215**. In an exemplary embodiment, the expansion of the anchoring conduit **200** enables the proximal anchor component **210** and the distal anchor component **215** to interface with a tissue component and define an open cavity **235** with a substantially uniform inner surface.

The terms proximal and proximate are used herein to describe a position which is in the relative vicinity of another position, including a range of vicinity positions through and including being directly adjacent or abutting another position. The term distal is used herein to describe a position which is situated a relative distance away from another position. Thus, the terms proximal/proximate and distal are used herein as spatial relation references and are not used to describe positions upstream or downstream in the flow of blood.

In the exemplary embodiment depicted in FIG. 2, the anchoring conduit **200** is deployed in an aortic valve **220**. The anchoring conduit **200** can be delivered in unexpanded state, thereby enabling endovascular delivery or other minimally invasive forms of deployment. Thus, in an exemplary embodiment, the anchoring conduit **200** can be percutaneously deployed via a catheter to the site of the aortic valve **220**. Once the surgeon, has delivered to the anchoring conduit **200** in a collapsed state to the desired location within the aortic valve **220**, the anchoring conduit **200** can then be expanded. It is this expansion of the anchoring conduit **200** that causes the proximal anchor component **210** to engage the lumen wall within the aorta **225**. In the exemplary embodiment shown in FIG. 2, the anchoring conduit **200** is positioned such that the proximal anchor component **210** engages the aortic valve **220** proximate the annulus of the aortic valve **220**. In this manner, the proximal anchor component **210** serves to collapse the cusps of the aortic valve **220** against the lumen wall of the aorta **225**. Thereby, the expansion of the anchoring conduit **200** may disable the native aortic valve **220**.

The expansion of the anchoring conduit **200** also serves to engage the distal anchor component **215** with the lumen wall of the aorta **225**. As shown in the exemplary embodiment of FIG. 2, the distal anchor component **215** can be positioned to engage the aorta **225** proximate the sinuses of the aorta **230**. In an exemplary embodiment, the anchoring conduit **200** can be configured to conform to the shape of the sinuses of the aorta **230** and thus aid in locking the anchoring conduit **200** into place. In an alternative embodiment, the distal anchor component **215** of the anchoring conduit **200** can be provided with hooks capable of piercing the lumen wall proximate the sinuses of the aorta **230**. The piercing of the lumen wall can aid in locking the anchoring conduit **200** in place.

An important advantage provided by an exemplary embodiment of the anchoring conduit **200** is that it can enable independent deployment of the valve anchor separate from

the deployment of a valve prosthesis. The independent deployment of the anchoring conduit **200** can help the surgeon avoid and minimize numerous risks involved in repairing a deficient heart valve. Conventional devices involve the percutaneous deployment of one device containing both the valve anchor and the valve prosthesis. Most often, the surgeon conducting a minimally invasive procedure is visually aided only by the two-dimensional sonographic image of an ultrasound. Thus, the surgeon is faced with the task of attempting to precisely implement a three-dimensional device with only two-dimensional feedback. When using a conventional device, the surgeon essentially has "one shot" to perfectly deploy the device.

The risks associated with the conventional "one shot" approach of percutaneous heart valve replacement are numerous and alarming. Unfortunately, many procedures performed with conventional devices have been unsuccessful and even fatal. A large risk associated with percutaneous deployment is that when the valve anchor of the conventional device is implemented on the hardened and calcified surface of the native valve, it can be loosely seated. A relatively loose seating of the conventional valve device may ultimately lead to migration of the device or leakage between the device and the lumen wall. Moreover, an additional risk results from the fact that the placement of the conventional device can breakup the calcium deposits on the deficient heart valve and release these deposits into the bloodstream. All of these risks are associated with the deployment of a conventional valve device. An exemplary embodiment of the anchoring conduit **200**, however, can help to minimize and avoid a number of these risks.

Contrary to conventional devices, the anchoring conduit **200** can contain only the anchoring components and inner lumen. The independent implementation of the anchoring conduit **200** permits the surgeon to concentrate on the variables involved in correctly and securely deploying the anchoring conduit **200** without concern for the placement or function of the replacement heart valve prosthesis. Therefore, the independent deployment of the anchoring conduit **200** can help to minimize the number of variables that the surgeon must control in deploying such a device. Furthermore, if the surgeon fails to correctly implement the anchoring conduit **200**, the surgeon can then implement certain procedures to correct the placement of the anchoring conduit **200** or extract the failed area where the anchoring conduit **200** was positioned. For example, and not limitation, should the placement of the anchoring conduit **200** fail, the patient can be placed on bypass and the failed aortic root can be replaced with an aortic root conduit.

As shown in FIG. 2, when the anchoring conduit **200** is been deployed in the aortic valve **220**, an open cavity **235** is created. This open cavity **235** can have a smooth and substantially uniform surface. This smooth and substantially uniform surface can replace the calcified, hardened, and rough surface of the deficient aortic valve **220**. The smooth and substantially uniform surface of the cavity **235** of the anchoring conduit **200** provides many advantages. Significantly, the smooth and substantially uniform surface of the cavity provides a greatly improved area for deploying a heart valve prosthesis. Conventional devices are often unsuccessful due to the necessity of anchoring the device on a non-uniform surface. Valve prosthesis deployed in accordance with an embodiment of the present invention can be enabled to be deployed on the substantially uniform inner surface of the anchoring conduit **200**.

In an exemplary embodiment the anchoring conduit **200** is composed of a thread-like structure that can be made of stainless steel, titanium, similar metals or metal alloys, or

suitable plastics. These thread-like structures or filaments can be latticed looped or wound. In one embodiment, the anchoring conduit **200** composed of a surgical stainless steel mesh. In some embodiments, the anchoring conduit **200** is composed of a shape memory material, such as a nickel-titanium alloy. The anchoring conduit **200** can be composed of a material capable of bending into the surface of the lumen wall against which it is anchored. As the native inner lumen is often an irregular and hard surface, is advantageous for the anchoring conduit **200** to be enabled to bend and conform to the shape of the native lumen wall against which it is anchored so as to ensure safe and secure seating of the anchoring conduit **200**. Additionally, an embodiment of the anchoring conduit **200** may include a biocompatible lumen. In this embodiment, the thread-like structure provides the outer core and its hollow interior can be lined with a biocompatible lumen. In some embodiments, the anchoring conduit **200** can provide an outer layer capable of bending to conform to the native lumen wall, and an inner layer which maintains a substantially uniform and smooth surface.

In alternative embodiments to that depicted in FIG. 2, the anchoring conduit **200** can be deployed in other areas of the aorta **225**. For example, and not limitation, the anchoring conduit **200** can be expanded such that the proximal anchor component **210** of the anchoring conduit **200** interfaces with the lumen wall of the aorta **225** proximate the sino-tubular junction. Therefore, the anchoring conduit **200** can be deployed further down on the aortic root. Additionally, the anchoring conduit **200** can be deployed further up the aorta, such as above the sinuses of the valsalva **230** or even proximate the aortic arch. Additionally, the anchoring conduit **200** can be deployed in valves other than aortic valve. In an exemplary embodiment, the anchoring conduit **200** can be deployed in a pulmonic valve.

FIG. 3 provides an illustration of an exemplary embodiment of anchoring conduit **200** and temporary valve **305** implemented in an aortic valve in accordance with an exemplary embodiment of the present invention. As shown in FIG. 3, the anchoring conduit **200** can be deployed in the aortic valve **220** such that the aortic valve **220** is disabled. More particularly, the expansion of the anchoring conduit **200** serves to collapse the cusps of the native aortic valve **220** and thus it ceases to function. In an exemplary embodiment of the present invention, a temporary valve **305** can be implemented to temporarily replace the function of this disabled heart valve.

The temporary valve **305**, in the exemplary embodiment shown in FIG. 3, can be a mechanical or bioprosthetic valve. The temporary valve **305** can be deployed in a minimally invasive manner, such as attached to a catheter **310** shown in FIG. 3. The temporary valve **305** can be initially collapsed while it is delivered to its functional location. When the temporary valve **305** is in its functional location, it can then be expanded. When the temporary valve **305** expands, it is pushed or sealed against the lumen wall of the aorta **225**. In an exemplary embodiment the temporary valve **305** does not attach to the wall of the aorta **225**. Once the temporary valve **305** is expanded, its cusps can open and close controlling the flow of blood through the aorta **225**. Therefore, the temporary valve **305** can be delivered before the native valve is rendered non-functional. Thus, once the native valve is rendered non-functional, the temporary valve **305** can perform the function of the native valve without interrupting the cardiac cycle of the beating heart.

FIG. 4A provides an illustration of an exemplary embodiment of a cardiac prosthetic system **400** implemented in aortic valve in accordance with an exemplary embodiment of the

present invention. As shown in FIG. 4A, the anchoring conduit **200** can be deployed in the aortic root proximate the aortic annulus. In an exemplary embodiment, the anchoring conduit **200** covers the inlet area between the left ventricle **430** and the aorta **225**. In one embodiment, the anchoring conduit **200** can cover an area immediately proximate the aortic annulus **405**.

In an exemplary embodiment shown in FIG. 4A, the anchoring conduit **200** can be delivered in a condensed form. For example, and not limitation, the anchoring conduit **200** can be composed of a surgical stainless mesh that is capable of being collapsed. The collapsed anchoring conduit **200** is capable of delivery in a minimally invasive manner, including via percutaneous deployment or a long arm delivery device. In an exemplary embodiment, an anchoring conduit **200** is delivered minimally invasively through a heart chamber or the arterial/venous system into the aortic root **410**. Once the collapsed anchoring conduit **200** is delivered to the desired location in the base of the aortic root **410** it can be expanded and anchored into the aortic root **410**. In an exemplary embodiment, the anchoring conduit **200** can be expanded proximate the aortic annulus **405**. In another embodiment, the anchoring conduit **200** can be expanded further into the aortic root **410**. Additionally, in an alternative embodiment, the steps of the methods of the present invention can be implemented via a remote device. For example, and not limitation, a surgeon could be enabled to use a remote device to expand the anchoring conduit **200** once delivered to the desired position.

In an exemplary embodiment, the anchoring conduit **200** provides a harbor **415**. The harbor **415** can include a releasably engaging component, which is enabled to serve as a receiving port for a heart valve prosthesis. This releasably engaging component, in an exemplary embodiment, is enabled to couple with a mating releasably engaging component of heart valve prosthesis **420**. The heart valve prosthesis **420** can be a variety of different types of heart valve prostheses, including various types of mechanical valves and bioprosthetic heart valves.

The implementation of the anchoring conduit **200** renders the native valve non-functional, therefore, an exemplary embodiment of the present invention provides a temporary valve that can be placed in the aorta **225** to perform the function of the native valve. The temporary valve **305**, in the exemplary embodiment shown in FIG. 4A, can be a mechanical or bioprosthetic valve. The temporary valve **305** can be deployed in a minimally invasive manner, such as attached to a catheter **310** shown in FIG. 4A. Therefore, the temporary valve **305** can be delivered before the native valve is rendered non-functional. Once the native valve is rendered non-functional, the temporary valve **305** can perform the function of the native valve without interrupting the cardiac cycle of the beating heart being repaired.

When both the anchoring conduit **200** and the temporary valve **305** are in place, the heart valve prosthesis **420** can be introduced into the heart. In an exemplary embodiment shown in FIG. 4A, the heart valve prosthesis **420** is introduced through a port **425** in the heart chamber. In an alternative embodiment, the heart valve prosthesis **420** can be introduced through the venous/arterial system. The port **425** in the exemplary embodiment depicted in FIG. 4A is mounted on the lower wall of the left ventricle **430** and provides an orifice through which the heart valve prosthesis **420** can be delivered. Those of skill in the art will appreciate that port **425** could be a variety of different ports known in the art. The heart valve prosthesis **420** can be delivered via a catheter or long arm device, or other minimally invasive apparatus. The heart

valve prosthesis 420 of the exemplary embodiment shown FIG. 4A is delivered via long arm device 435.

In the exemplary embodiment depicted in FIG. 4A, once the heart valve prosthesis 420 has been introduced into the left ventricle 430, it can be delivered to a harbor 415 on the anchoring conduit 200. In an exemplary embodiment, the heart valve prosthesis 420 includes a plurality of leaflets 440. These leaflets 440 can function to replace the action of deficient heart valve. Additionally, the heart valve prosthesis 420 provides an annulus ring 445. The annulus ring 445 is capable of interfacing with the anchoring conduit 200 to provide a proper seal for the heart valve prosthesis 420. The heart valve prosthesis 420 may be stented or stentless according to needs of particular implementation.

In an exemplary embodiment, the heart valve prosthesis 420 can provide a releasably engaging component. This releasably engaging component is enabled to couple and uncouple to a mating releasably engaging component provided on harbor 415. The releasably engaging component of the heart valve prosthesis 420 can be positioned at various locations on the device to ensure proper mating with the harbor 415. This releasably engaging component may be on the annulus or stent portion of the heart valve prosthesis 420. Once the heart valve prosthesis 420 has been mated to the releasably engaging component of the harbor 415 of the anchoring conduit 200, the harbor 415 can releasably retain the heart valve prosthesis 420 in place, and the heart valve prosthesis 420 can be released from the catheter or long arm.

After heart valve prosthesis 420 is deployed, the temporary valve 305 can be extracted. Furthermore, the ports in the venous/arterial system or ports in the heart can be closed using a mechanism which can allow them to be opened when the heart valve needs to be replaced.

When a heart valve prosthesis 420 fails or reaches a limit in its functional life, the ports in the arterial/venous system and the heart chambers can be reopened to deliver a new heart valve prosthesis to the harbor 415 in the anchoring conduit 200. Again, a temporary valve 305 can be placed in the aorta 225 to control blood flow. Then, a catheter or long arm can be used to engage the old heart valve prosthesis 420 on the anchoring conduit 200. The heart valve prosthesis 420 can then be uncoupled from the releasably engaging component of the harbor 415 and the old heart valve prosthesis 420 can be extracted. A new heart valve prosthesis can subsequently be introduced into the left ventricle 430, via a catheter or long arm mechanism, and releasably engaged to the harbor 415 of anchoring conduit 200. Thus, the deficient heart valve prosthesis can be replaced with a new heart valve prosthesis in a minimally invasive manner. The above process may be repeated one or several times over the life of the patient according to clinical requirements.

FIG. 4B provides an illustration of an alternative embodiment of a cardiac prosthetic system 400 implemented in aortic valve in accordance with an exemplary embodiment of the present invention. In the alternative embodiment depicted in FIG. 4B, the heart valve prosthesis 420 is delivered via a conduit in the temporary valve 305. In the alternative embodiment shown in FIG. 4B, the temporary valve 305 is delivered via an enlarged catheter 450 which provides an internal conduit 455. The internal conduit 455 enables a path through which a heart valve prosthesis 420 can be delivered in accordance with an exemplary embodiment of the cardiac prosthetic system 400.

As shown in FIG. 4B, the alternative embodiment of the heart valve prosthesis 420 is enabled to be passed through the center of the temporary valve 305. Thereby, in accordance with a method of improving a deficient heart valve of the

present invention, the temporary valve 305 can be deployed to temporarily perform the function of the deficient aortic valve 220. The anchoring conduit 200 can then be properly seated and secured within the deficient aortic valve as shown in FIG. 4B. After it is verified that the anchoring conduit 200 has been properly placed, the heart valve prosthesis 420 can then be delivered to the aorta 225 via the internal conduit 455 of the enlarged catheter 450. In an exemplary embodiment, the heart valve prosthesis 420 is capable of delivery in a collapsed form, such that it can be passed through the internal conduit 455. Once the heart valve prosthesis 420 has entered the aorta 225, it can be expanded into functional form. Thereafter, the heart valve prosthesis 420 can be deployed in the anchoring conduit 200.

In the embodiment depicted in FIG. 4B, a releasably engaging component on the heart valve prosthesis 420 can be coupled to a mating releasably engaging component on the harbor 415 of the anchoring conduit 200. In an alternative embodiment, the heart valve prosthesis 420 can be provided without a releasably engaging component. In this alternative embodiment, the heart valve prosthesis 420 can simply be expanded within the anchoring conduit 200 such that the annulus 445 of the heart valve prosthesis 420 interfaces with the smooth inner surface of the anchoring conduit 200. Those of skill in the art will appreciate that the heart valve prosthesis 420 could be delivered and deployed in a number of different manners without detracting from the scope of the invention.

An additional alternative embodiment of the cardiac prosthetic system 400 enables an alternative method for the delivery of the anchoring conduit 200. In this embodiment, the anchoring conduit 200 is enabled to be delivered through the internal conduit 455 of the enlarged catheter 450 shown in FIG. 4B. Thus, the method of improving a deficient heart valve implemented with this embodiment can first involve the delivery and deployment of the temporary valve 305 to an area proximate the deficient heart valve. Next, the anchoring conduit 200 can be permitted to pass through the internal conduit 455 of the enlarged catheter 450 of the deployed temporary valve 305. Thus, the anchoring conduit 200 can be delivered by catheter in a compressed state through the temporary valve 305. The anchoring conduit 200 can then be positioned proximate the deficient heart valve and deployed. After the anchoring conduit 200 is successfully deployed, the catheter that delivered the anchoring conduit 200 can be removed. Subsequently, a heart valve prosthesis 420 can be delivered through the internal conduit 455 of the enlarged catheter 450 of the deployed temporary valve 305.

FIG. 5A provides an illustration of an exemplary embodiment of an anchoring conduit 200 in accordance with an exemplary embodiment of the present invention. The anchoring conduit 200 has a proximal anchor component 210 and a distal anchor component 215. The proximal anchor component 210 can be anchored into a lumen wall. In the exemplary embodiment depicted in FIG. 5A, the proximal anchor component 210 has a flared edge which serves as a seal preventing leaks between the aortic root and the walls of the anchoring conduit 200. In an exemplary embodiment, the distal anchoring edge 215 is contoured to the shape of the sinuses of the aorta 230. In this exemplary embodiment, the distal anchoring edge 215 is configured to engage the surface of the sinuses of the aorta 230 and further secure the anchoring conduit 200 into place.

Additionally, the exemplary embodiment of the anchoring conduit 200 shown in FIG. 5A provides tissue piercing components 505 and 510. The tissue piercing components 505 and 510 are enabled to pierce and engage a tissue component, and, thus, aid in stabilizing the anchoring conduit 200. In the

exemplary embodiment shown in FIG. 5A, the piercing components **505** and **510** of the distal anchor component **220** flare into the sinuses of valsalva and help to secure the anchoring conduit **200** into place. Those of skill in the art will appreciate that the piercing components **505** and **510** can be hooks or other types of anchors sufficient to engage a tissue component in the heart. The expansion into the sinuses may have a lumen in order to prevent blood migration between the conduit and the aortic wall. In an exemplary embodiment, the anchoring conduit **200** provides an outer surface for mating with the irregularities of the surface to which the anchoring conduit **200** is seated and a substantially uniform inner surface. Thereby, the smooth and substantially uniform inner surface of the anchoring conduit **200** is not effected by the undulations impressed in the seated outer surface of the anchoring conduit **200**.

As shown in FIG. 5A, and exemplary embodiment of the anchoring conduit **200** can provide a releasably engaging component **515**. The releasably engaging component **515** can be many suitable components capable of enabling the coupling and uncoupling of a heart valve prosthesis **420**. The releasably engaging component **515** shown in the exemplary embodiment in FIG. 5A is comprised of threading. Thus, the proximal anchor component **210** can provide a series of threading for the releasably engaging component **515**. Coupling of the heart valve prosthesis **420** can then be accomplished, in the exemplary embodiment, by attaching a mating releasably engaging component of the heart valve prosthesis **420** with appropriate counter threading. Therefore, the method of improving a deficient heart valve in accordance with the present invention can involve the coupling of heart valve prosthesis **420** to the threading of the releasably engaging component **515** of the anchoring conduit **200**. Those of skill in the art will appreciate that number of different devices, components, and mechanisms could be substituted for the threading of the releasably engaging component **515** shown in FIG. 5A without detracting from the invention. For example, and not limitation, the releasably engaging component **515** could be a series of groves in which mating prongs can be inserted, an orifice through which an expanding toggle component can be inserted, a magnetic system, clamps, a latching mechanism, or other suitable component.

FIG. 5B provides an illustration of an exemplary embodiment of an anchoring conduit **200** in accordance with an exemplary embodiment of the present invention. In the exemplary embodiment depicted in FIG. 5B, the anchoring conduit **200** traverses the sinuses of the valsalva **230**. As previously described in relation to FIG. 1, the sinuses of the valsalva **230** are located just above the three cusps, **105**, **110**, and **115** (FIG. 1) and each sinus corresponds to each individual cusp. Proximate the sinuses of the valsalva **230** are the origins of the coronary arteries. The anchoring conduit **200** can provide openings proximate the sinuses of the valsalva so as not to interrupt the openings to the coronary arteries and allow for the free flow of blood. In the exemplary embodiment shown in FIG. 5B, the distal anchor component **215** of the anchoring conduit **200** may also extend beyond the sinuses of valsalva **230** and anchor into the aortic wall below the aortic arch, as shown in FIG. 5B.

In the exemplary embodiment shown in FIG. 5B, an external aortic ring **520** may be releasably placed on the external surface of the aortic root in order to aid in locking the anchoring conduit **200** in place. In this embodiment, the distal anchor component **210** of anchoring conduit **200** protrudes radially outward against the lumen wall. The aortic ring **520** can then be deployed below the protrusions in the distal anchor

component **350** of the anchoring conduit **200**, and thereby prevent the anchoring conduit **200** from migrating past the aortic ring **520**.

The exemplary embodiment of the anchoring conduit **200** shown in FIG. 5B provides a proximal anchor component **210**. The proximal end **210** can contain a harbor **415**. The harbor **415** can enable the releasable connection of a heart valve prosthesis. The harbor **415** in the exemplary embodiment in FIG. 5B is placed on the proximal anchor component **210** of the anchoring conduit **200**. In another embodiment, the harbor **415** may be located in the normal position of the native valve. In an alternative embodiment, the harbor **415** can be located in the distal anchor component **215** of the anchoring conduit **200**. The harbor **415** can provide a releasably engaging component. Those of skill in the art will appreciate that many different types of releasably engaging components could be incorporated into the harbor **415** to accomplish the necessary function.

FIG. 6 provides an illustration of an exemplary embodiment of a temporary valve **305** in accordance with an exemplary embodiment of the present invention. The temporary valve **305** includes a single or plurality of leaflets within a collapsible frame. In the exemplary embodiment shown in FIG. 4, the leaflets **605** can be constructed of biocompatible materials. In a non-limiting example, a biocompatible polymer material is used to create the leaflets **605**. In an alternative embodiment, the leaflets **605** of the temporary valve **305** can be constructed from bovine pericardium. In yet another embodiment, the leaflets **605** of the temporary valve **305** can be constructed from porcine aortic leaflets. Additionally, the leaflets **605** of the temporary valve **305** can be constructed from metallic materials such as carbon or other metals. Those of skill in the art will appreciate that the temporary valve **305** can be a number of different types of valves capable of temporary deployment into the heart.

In the exemplary embodiment depicted in FIG. 4, the collapsible frame **610** of the temporary valve **305** may be constructed of a biocompatible polymer structure. In another embodiment, the collapsible frame **610** may be constructed using a doughnut shaped balloon, where the balloon is constructed of a polymer. Alternatively, an embodiment of the collapsible frame **610** may be constructed of a memory alloy or memory polymer mesh.

As shown in FIG. 6, the collapsible frame **610** can be attached to a polymer catheter **615** for delivery to the desired location within the heart. Typically the collapsible frame **610** is permanently connected to the catheter **310**, as it is not necessary to release the collapsible frame **610** from the catheter **310**. The catheter **310** enables a surgeon to maintain control over the function and location of the temporary valve **305**. Moreover, the catheter **310** can cause the collapsible frame **610** and leaflets **605** to collapse under direct control of the surgeon. For example, and not limitation, if the anchoring conduit is to be positioned in the native aortic valve, the temporary valve **305** can be endovascularly delivered via catheter **310** to a position proximate the native aortic valve in the aorta. Thus, the temporary valve **305** can be expanded and deployed to replace the function of the native aortic valve before the anchoring conduit renders the native aortic valve nonfunctional.

FIG. 7 provides an illustration of an exemplary embodiment of a heart valve prosthesis **420** in accordance with an exemplary embodiment of the present invention. The heart valve prosthesis **420** in its preferred embodiment is a bioprosthetic valve. The heart valve prosthesis **420** includes a single or plurality of leaflets **705**. In an exemplary embodiment, the leaflets **705** may be constructed of treated tissue, such as but

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not limited to, bovine pericardium or aortic leaflet material. In other embodiments the leaflets **705** may be constructed of a biocompatible polymer.

As shown in FIG. 7, the heart valve prosthesis **420** can have an annulus **710**. The annulus **710** may be constructed of biocompatible metals or polymers. Additionally, as shown in FIG. 7, the heart valve prosthesis **420** has a releasably engaging component **715**. The releasably engaging component **715** is enabled to be coupled to the releasably engaging component of harbor **415**. Thereby, the releasably engaging component **715** of the heart valve prosthesis **420** can be securely attached to the harbor **415**. In an exemplary embodiment shown in FIG. 7, the releasably engaging component **715** of the heart valve prosthesis **420** is threading, which can be provided on the side of the heart valve prosthesis **420**. The threading of the releasably engaging component **715** can couple to counter-threading of the releasably engaging component **515** (FIG. 5A) of the anchoring conduit **200**. Those of skill in the art will appreciate that the releasably engaging component **715** may be many other suitable components including, but not limited to, a screw, magnetic, clamps or latching systems which can releasably engage the heart valve prosthesis **420** with the harbor **415**.

The heart valve prosthesis **420** can also be enabled to be connected to a catheter or long arm which may be used to deliver the arm to a specific location. In its preferred embodiments the catheter or long arm device which releasably attaches a heart valve prosthesis **420** into the harbor **415**, may be constructed of a biocompatible polymer or metal. The long arm device has distal and proximal ends. In the distal end, the catheter or long arm device has a locking component which may releasably hold a heart valve prosthesis **420**. This locking component may be a screw, clamp, latching system, or many other suitable components. On the proximal end, the long arm device or catheter contains a control component which can allow the release or coupling of a heart valve. Additionally the long arm device or catheter is controllably flexible in order to direct the heart valve prosthesis **420** to the desired location.

FIG. 8 provides an illustration of an exemplary embodiment of a cardiac prosthetic system **400** implemented in a pulmonic valve in accordance with an exemplary embodiment of the present invention. As shown in FIG. 8, the anchoring conduit **200** can be deployed in the pulmonary artery **815** proximate the pulmonic valve **805**. In an exemplary embodiment, the anchoring conduit **200** covers the inlet area between the right ventricle **810** and the pulmonary artery **815**. In one embodiment, the anchoring conduit **200** can be implemented in an area immediately proximate the pulmonic valve **805**. In alternate embodiment, the anchoring conduit **200** can be implemented over a larger portion of the pulmonary artery **815**. Those of skill in the art will appreciate that the dimensions and placement location of the anchoring conduit **200** can be modified in a variety of embodiments without detracting from the scope of the invention.

In an exemplary embodiment, the anchoring conduit **200** provides a harbor **415**. The harbor **415** can include a releasably engaging component, which is enabled to serve as a receiving port for a heart valve prosthesis **420**. The implementation of the anchoring conduit **200** renders the native pulmonic valve **805** non-functional, therefore, an exemplary embodiment of the present invention provides a temporary valve **305** that can be placed in the pulmonary artery **815** to perform the function of the native pulmonic valve **805**.

When both the anchoring conduit **200** and the temporary valve **305** are in place, the heart valve prosthesis **420** can be introduced into the heart. In an exemplary embodiment, the heart valve prosthesis **420** is introduced through a port **820** in

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the heart chamber. The port **820** in the exemplary embodiment depicted in FIG. 8 is mounted on the lower wall of the right ventricle **810** and provides an orifice through which the heart valve prosthesis **420** can be delivered. In the exemplary embodiment depicted in FIG. 8, once the heart valve prosthesis **420** has been introduced into the right ventricle **810**, it can be delivered to a harbor **415** on the anchoring conduit **200**.

In an exemplary embodiment, the heart valve prosthesis **420** can provide a releasably engaging component enabled to couple to a mating releasably engaging component provided on harbor **415**. Once the heart valve prosthesis **420** has been mated to the releasably engaging component of the harbor **415** of the anchoring conduit **200**, the harbor **415** can releasably retain the heart valve prosthesis **420**, and the heart valve prosthesis **420** can be released from the catheter or long arm.

After heart valve prosthesis **420** is in place, the temporary valve **305** can be extracted. Furthermore, the ports in the venous/arterial system or ports in the heart can be closed in a manner that can allow them to be opened if the heart valve needs to be replaced. Thereby, should the first heart valve prosthesis deployed become deficient, a second heart valve prosthesis can be replaced for the first.

While the invention has been disclosed in its preferred forms, it will be apparent to those skilled in the art that many modifications, additions, and deletions can be made therein without departing from the spirit and scope of the invention and its equivalents as set forth in the following claims.

What is claimed is:

1. A method of preparing a heart valve for replacement comprising:
  - delivering an anchoring conduit to a heart valve, the anchoring conduit comprising an expandable structure having an outer layer and an inner layer, the outer layer configured to bend to conform to the contour of a tissue component and the inner layer comprising a smooth and substantially uniform inner surface;
    - wherein the expansion of the expandable structure enables the expandable structure to interface with the tissue component and define an open cavity, the open cavity defined at least in part by the inner layer having the smooth and substantially uniform inner surface;
    - wherein the anchoring conduit includes a harbor enabled to releasably connect a heart valve prosthesis; and
    - expanding the anchoring conduit in the heart valve.
2. The method of preparing a heart valve for replacement of claim 1 further comprising:
  - delivering a temporary valve, in a condensed state, to a target site proximate the heart valve; and
  - deploying the temporary valve at the target site proximate the heart valve; and
  - wherein the temporary valve operates to temporarily replace the function of the heart valve when the anchoring conduit is expanded.
3. The method of preparing a heart valve for replacement of claim 1, wherein the open cavity of the anchoring conduit provides an inner lumen surface against which a heart valve prosthesis can be deployed.
4. The method of preparing a heart valve for replacement of claim 1, wherein the inner surface of the open cavity includes a biocompatible lumen.
5. An anchoring conduit comprising:
  - an expandable structure having an outer layer and an inner layer, the outer layer configured to bend to conform to the contour of a tissue component and the inner layer comprising a smooth and substantially uniform inner surface;

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wherein the expansion of the expandable structure enables the expandable structure to interface with the tissue component and define an open cavity, the open cavity defined at least in part by the inner layer having the smooth and substantially uniform inner surface; and wherein the anchoring conduit, further comprises a harbor in communication with the expandable structure, the harbor including a first releasably engaging component.

6. The anchoring conduit of claim 5, wherein the anchoring conduit further comprises an anchoring component configured to disable a heart valve.

7. The anchoring conduit of claim 5, wherein the anchoring conduit further comprises an anchoring component configured to disable a native heart valve by compressing the components of the native heart valve against the native heart valve.

8. The anchoring conduit of claim 5, wherein an anchoring component is configured to receive a heart valve prosthesis.

9. The anchoring conduit of claim 8, wherein the expandable structure is configured to enable tissue growth onto the heart valve prosthesis.

10. The anchoring conduit of claim 5, wherein an anchoring component is enabled to be endovascularly delivered.

11. The anchoring conduit of claim 5, wherein a heart valve prosthesis having a second releasably engaging component is enabled to be securely coupled and uncoupled from the first releasably engaging component of the harbor.

12. The anchoring conduit of claim 11, wherein the heart valve prosthesis can be coupled and uncoupled from the first releasably engaging component of the harbor within the heart.

13. The anchoring conduit of claim 5, wherein the expandable structure is configured to contain a plurality of debris released from the tissue component.

14. The anchoring conduit of claim 5, wherein the expandable structure is configured to expand and adapt to the geometry of the sinuses of the valsalva.

15. The anchoring conduit of claim 5, wherein the anchoring conduit can be delivered through the apex of a heart.

16. The anchoring conduit of claim 5, wherein the expandable structure comprises a proximal anchor component and a distal anchor component.

17. The anchoring component of claim 16, wherein the proximal anchor component and the distal anchor component are configured to interface with the tissue component.

18. A method of improving a valve competency comprising:

providing the anchoring conduit of claim 5 to an area proximate a heart valve, wherein the harbor is enabled to releasably connect a heart valve prosthesis;  
 deploying the anchoring conduit, the deployment of the anchoring conduit defining the open cavity; and  
 deploying a heart valve prosthesis in the open cavity of the anchoring conduit.

19. The method of improving a valve competency of claim 18, wherein deploying the heart valve prosthesis involves expanding the heart valve prosthesis within the open cavity of the anchoring conduit.

20. The method of improving a valve competency of claim 18, wherein the anchoring conduit provides a first releasably engaging component and the heart valve prosthesis provides a second releasably engaging component enabled to be securely coupled and uncoupled from the first releasably engaging component of the anchoring conduit.

21. The method of improving a valve competency of claim 20, wherein deploying the heart valve prosthesis involves securely coupling the second releasably engaging component

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of the heart valve prosthesis to the first releasably engaging component of the anchoring conduit.

22. The method of improving a valve competency of claim 21, further comprising:

removing the heart valve prosthesis from the anchoring conduit; and  
 deploying a second heart valve prosthesis in the open cavity of the anchoring conduit.

23. A method of improving a deficient heart valve comprising:

delivering the anchoring conduit of claim 5 to a heart valve; delivering a temporary valve, in a condensed state, to a target site proximate the heart valve;  
 deploying the temporary valve at the target site proximate the heart valve; and  
 deploying the anchoring conduit in the heart valve, the deployment of the anchoring conduit disabling the heart valve; and

wherein the temporary valve operates to temporarily replace the function of the heart valve when the anchoring conduit is expanded.

24. The method of improving a deficient heart valve of claim 23, further comprising:

delivering the heart valve prosthesis to an area in the heart proximate the anchoring conduit; and  
 coupling the heart valve prosthesis to the harbor of the anchoring conduit.

25. The method of improving a deficient heart valve of claim 24, further comprising removing the temporary valve.

26. The method of improving a deficient heart valve of claim 25, further comprising:

delivering a temporary valve, in a condensed state, to a target site in an artery proximate the heart valve;  
 expanding the temporary valve at the target site in the artery proximate the heart valve;  
 decoupling the heart valve prosthesis from the harbor of the anchoring conduit;

delivering a second heart valve prosthesis to an area in the heart proximate the anchoring conduit; and

coupling the second heart valve prosthesis to the harbor of the anchoring conduit.

27. The method of improving a deficient heart valve of claim 26, further comprising removing the temporary valve.

28. The method of improving a deficient heart valve of claim 24, wherein the temporary valve and the heart valve prosthesis are endovascularly delivered.

29. The method of improving a deficient heart valve of claim 28, wherein the heart valve prosthesis can be delivered through a conduit in the temporary valve.

30. The method of improving a deficient heart valve of claim 23, wherein the heart valve is an aortic valve.

31. The method of improving a deficient heart valve of claim 23, wherein the heart valve is a pulmonic valve.

32. A cardiac prosthetic system comprising:

the anchoring conduit of claim 5; a temporary valve; and  
 a heart valve prosthesis having a second releasably engaging component enabled to be securely coupled and uncoupled from the first releasably engaging component of the harbor.

33. The cardiac prosthetic system of claim 32, further comprising a second heart valve prosthesis, the second heart valve prosthesis having a third releasably engaging component enabled to be coupled and uncoupled from the first releasably engaging component of the harbor.

34. The cardiac prosthetic system of claim 32, wherein the anchoring conduit is enabled to be deployed in an aortic heart valve.

35. The cardiac prosthetic system of claim 32, wherein the anchoring conduit is enabled to be deployed in a pulmonic heart valve.

36. The cardiac prosthetic system of claim 32, wherein the anchoring conduit is enabled to be delivered through a blood vessel.

37. The cardiac prosthetic system of claim 32, wherein the temporary valve is enabled to temporarily perform the function of a heart valve.

38. The cardiac prosthetic system of claim 32, wherein the temporary valve and the heart valve prosthesis are endovascularly delivered.

39. The cardiac prosthetic system of claim 38, wherein the heart valve prosthesis can be delivered through a conduit in the temporary valve.

40. A cardiac device comprising:  
 a heart valve prosthesis having a releasably engaging component; and  
 the anchoring conduit of claim 5; wherein the releasably engaging component is enabled to be connected to the harbor located within a heart.

41. The cardiac device of claim 40, wherein the releasably engaging component of the harbor is capable of being coupled to the releasably engaging component of the heart valve prosthesis.

42. The cardiac device of claim 40, wherein the heart valve prosthesis is enabled to be released from its connection to the harbor located within the heart.

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