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- (54) **NEURAL INTERFACING DEVICE**
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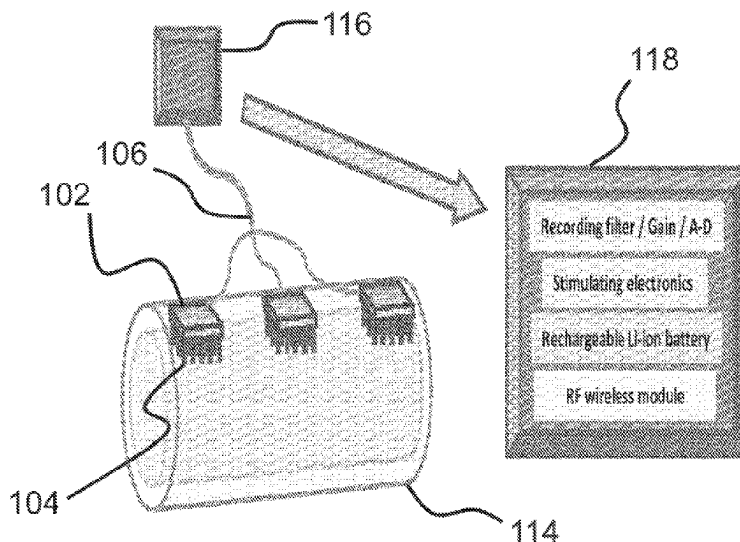
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- (57) **ABSTRACT**
A neural interfacing device is disclosed. The neural interfacing device may include at least one microneedle electrode. The microneedle electrode may have one or more microneedles. The one or more microneedles may be shaped and positioned such that when the neural interfacing device is applied to a nerve, the one or more microneedles penetrate a nerve epineurium without any portion of the microneedle electrode penetrating any nerve axon beyond a depth of 500 micrometers.

22 Claims, 9 Drawing Sheets



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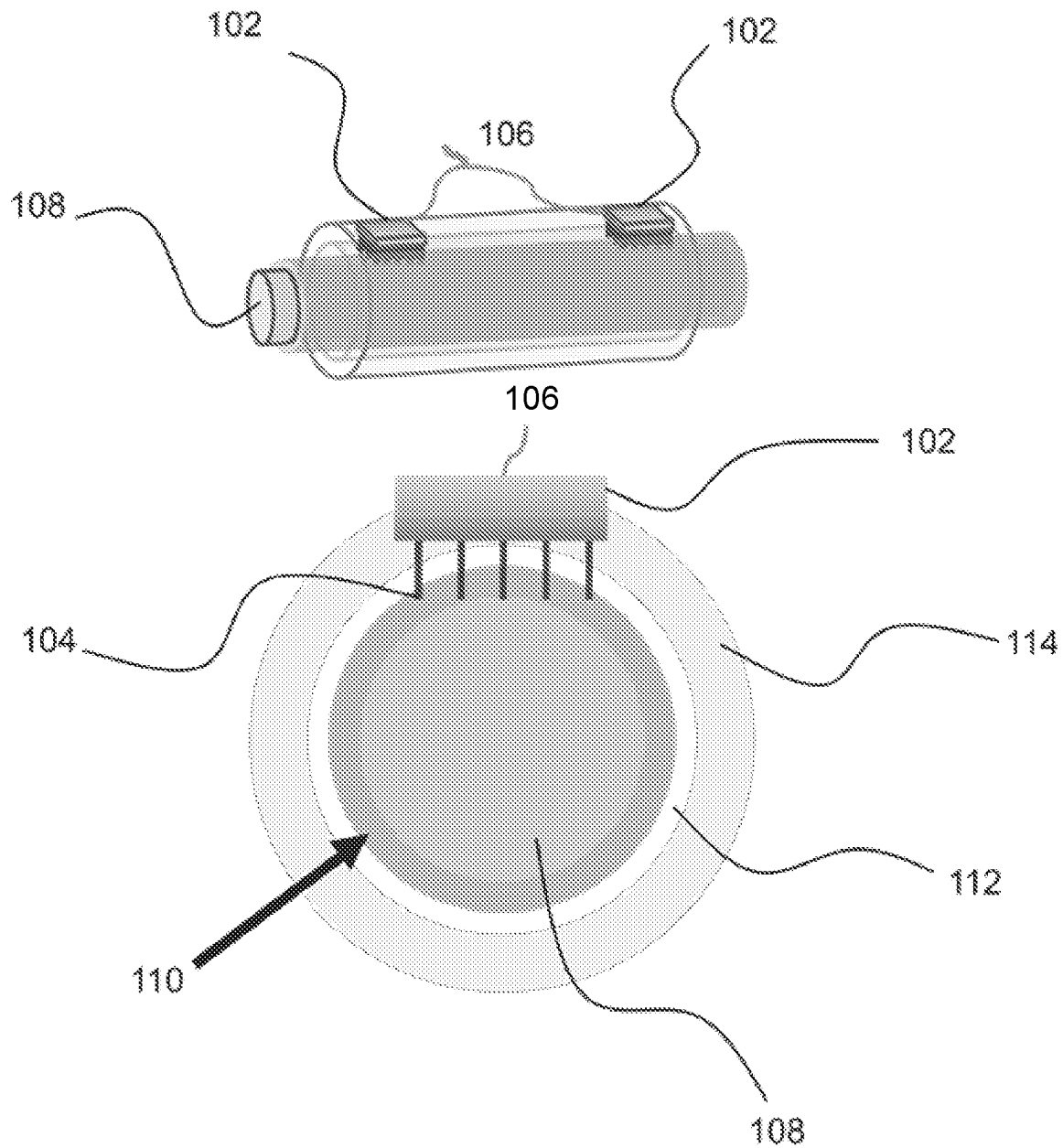


Fig. 1

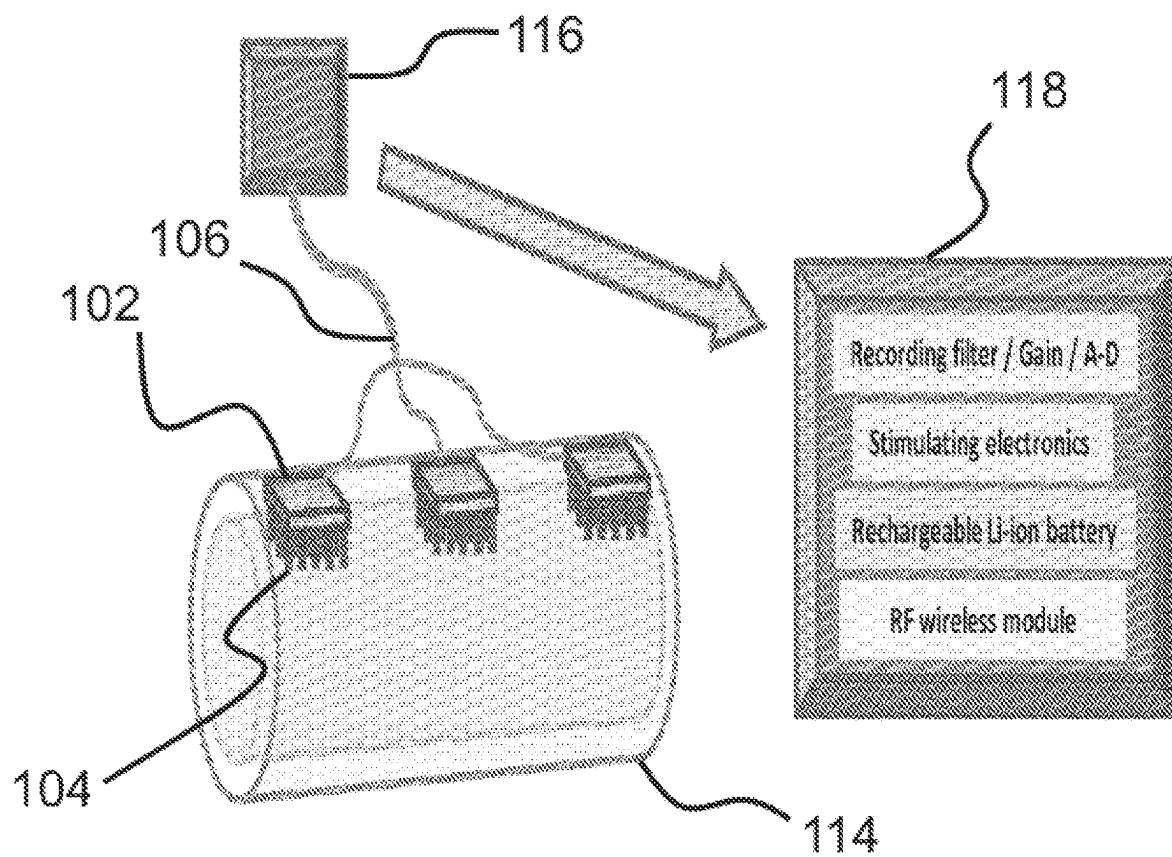
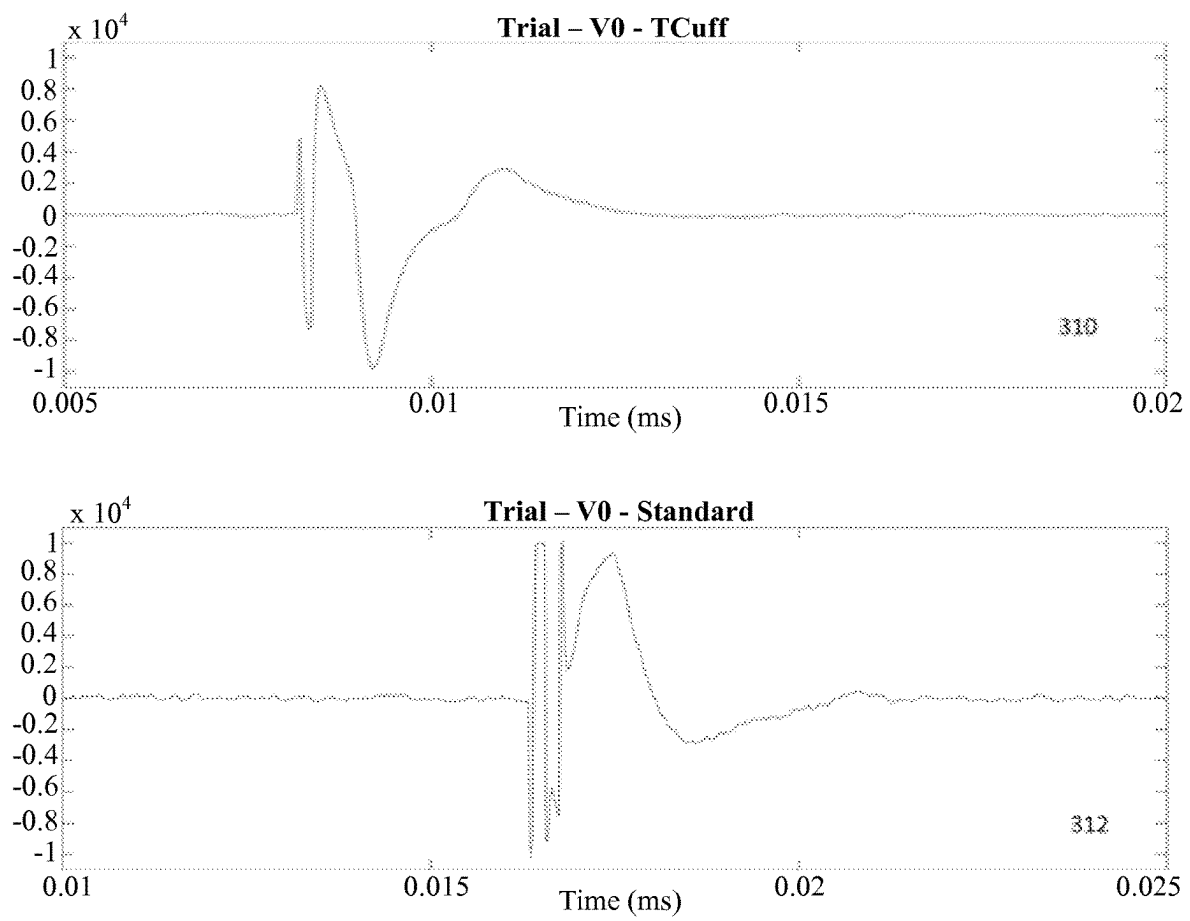


Fig. 2

**Fig. 3**

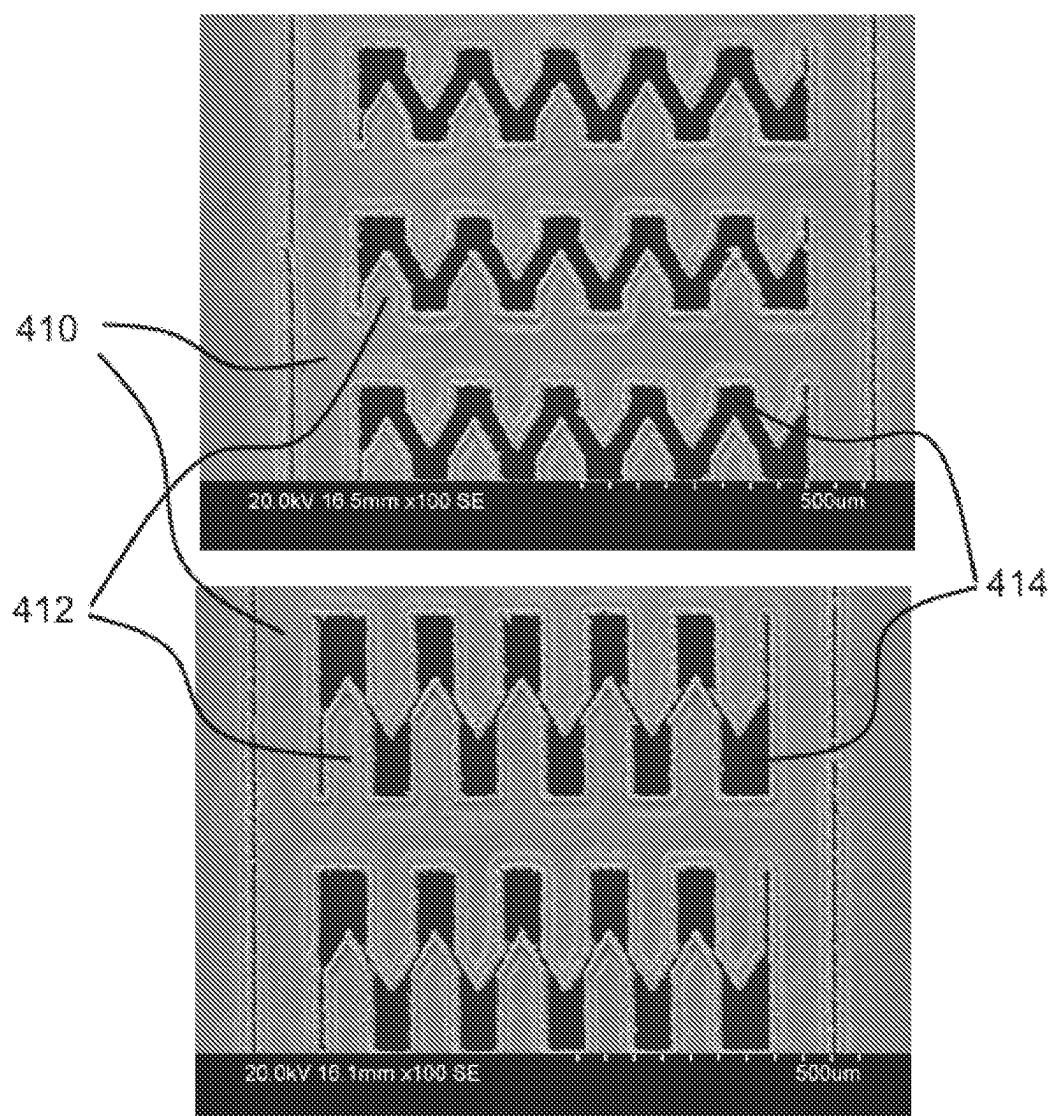


Fig. 4

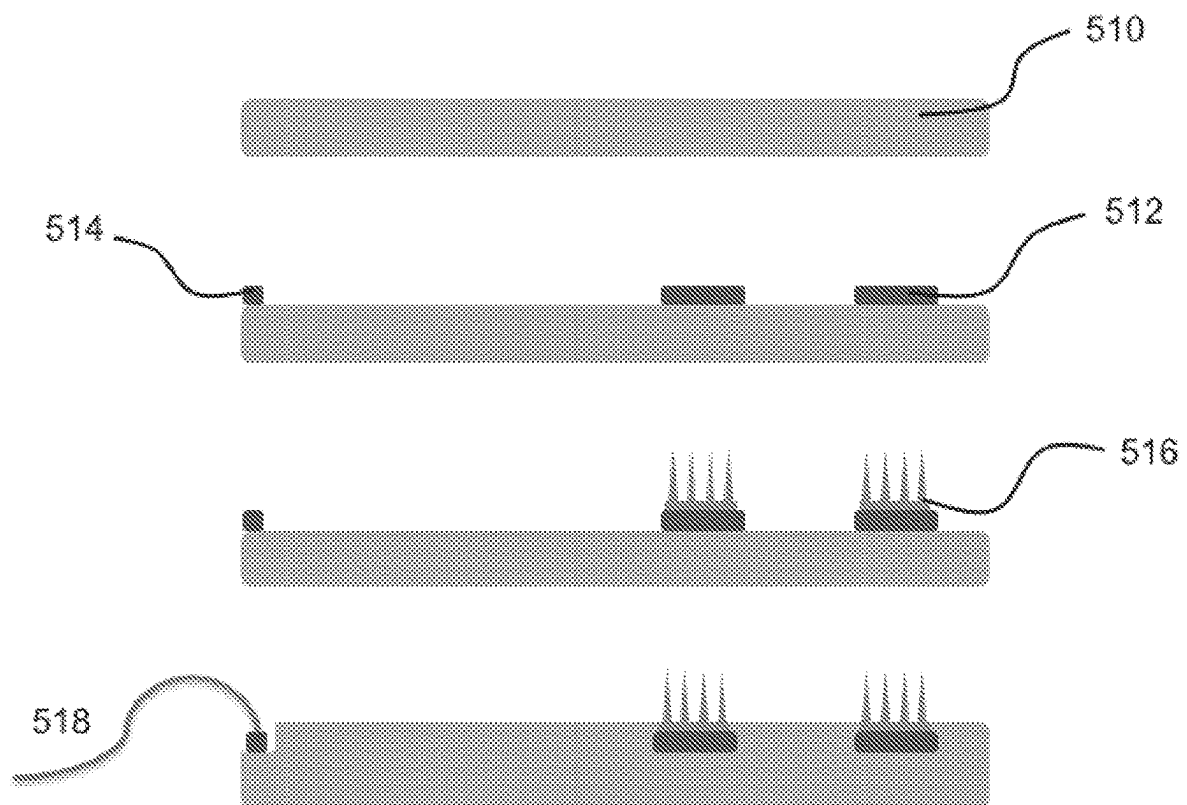


Fig. 5

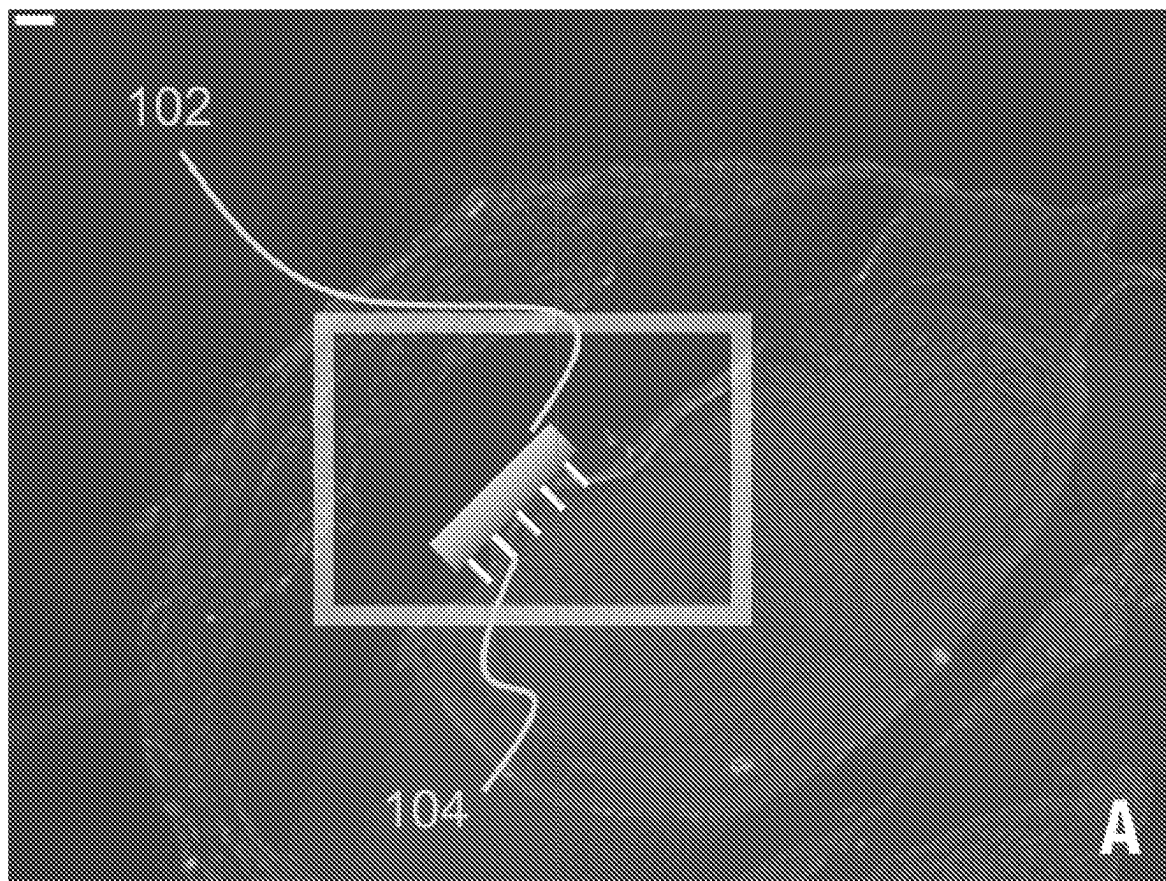
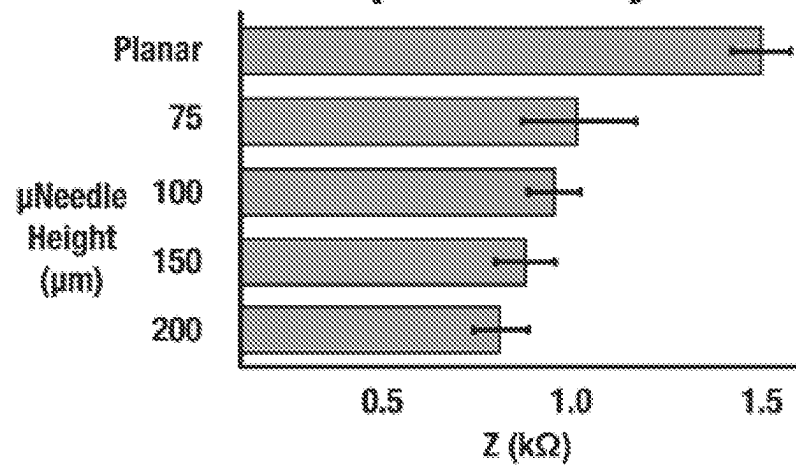
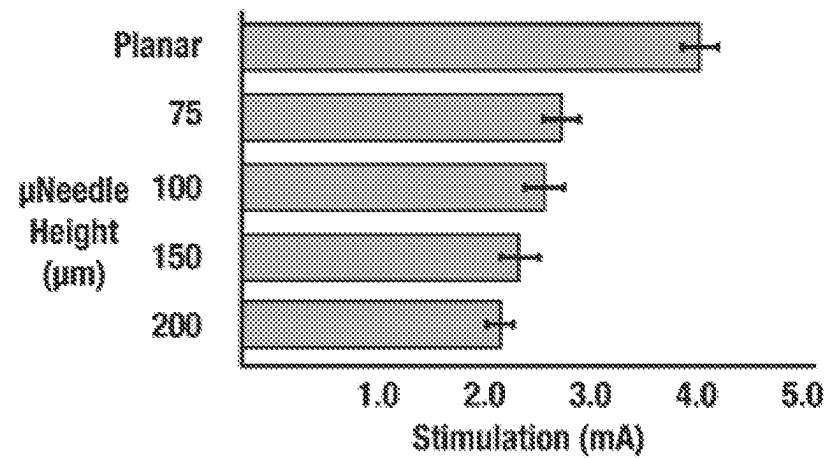
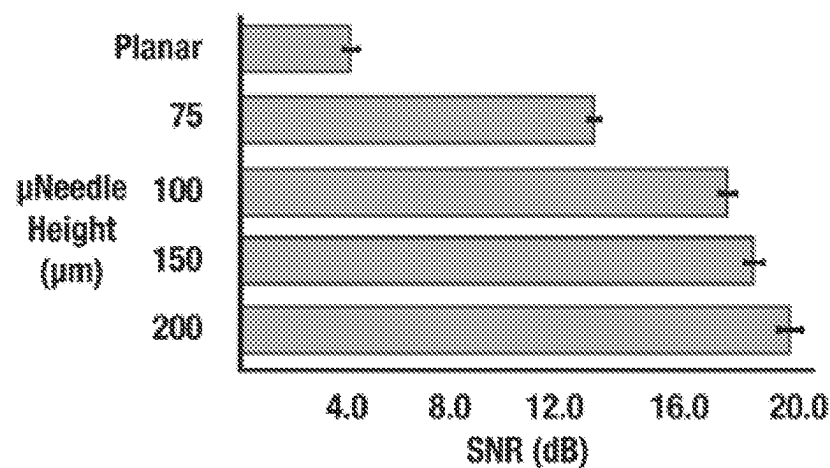


Fig. 6

Nerve-electrode impedance analysis**Stimulation thresholds****Recordings (signal-to-noise)****Fig. 7**

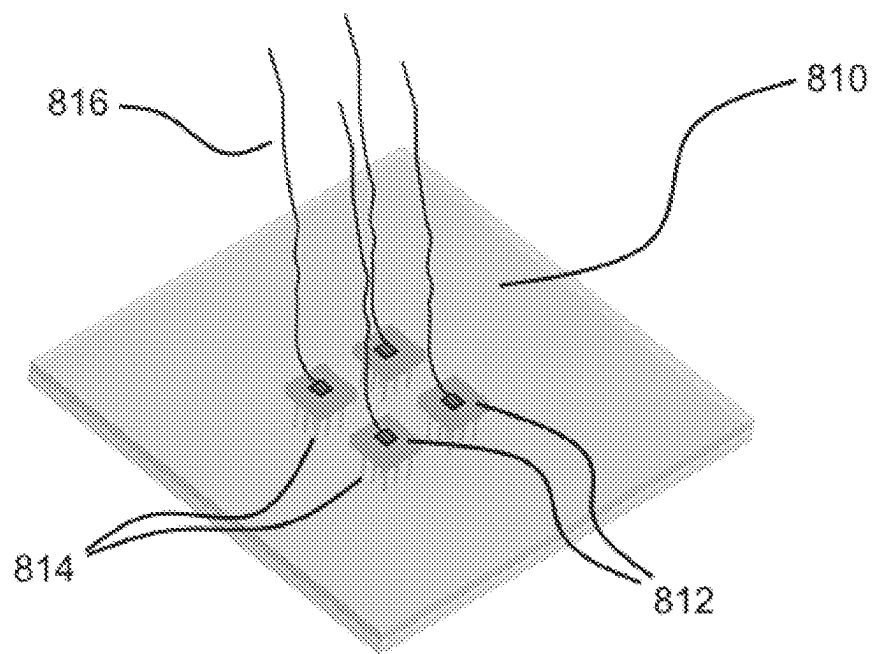


Fig. 8

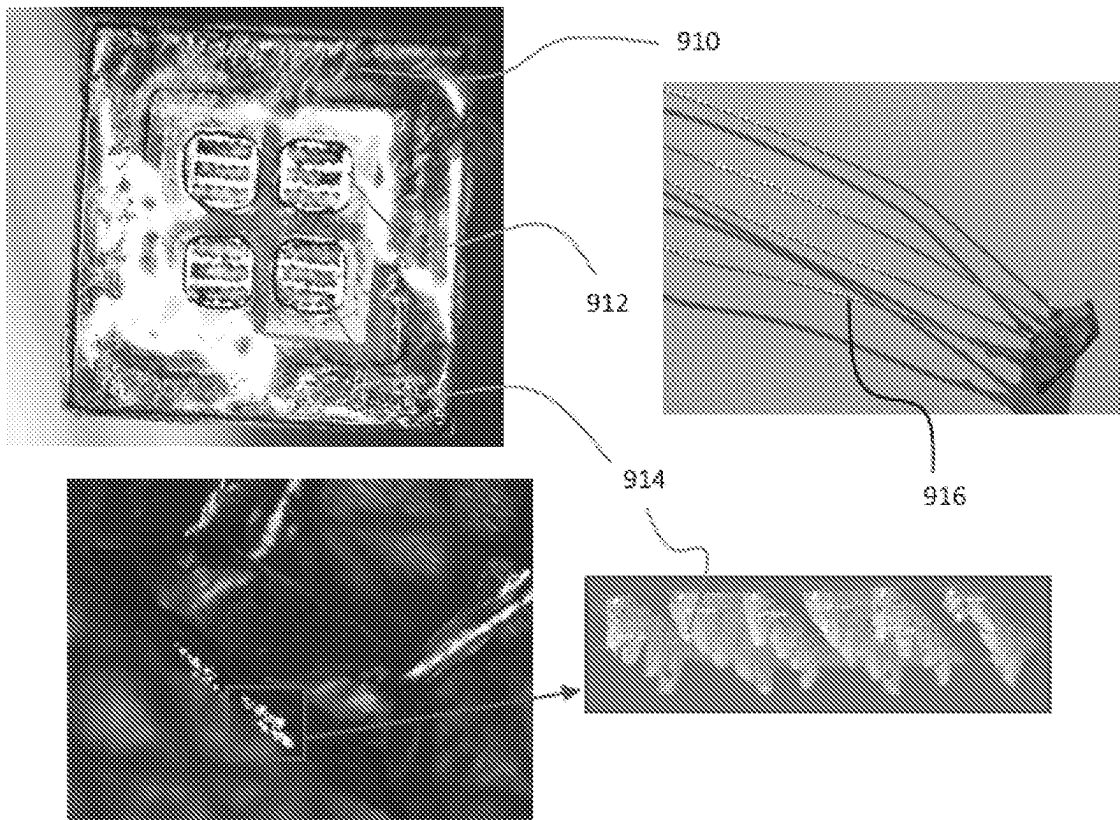


Fig. 9

NEURAL INTERFACING DEVICE

This application claims priority to U.S. Provisional Patent Application No. 61/934,708, filed on Feb. 1, 2014, and hereby incorporated by reference in its entirety.

BACKGROUND OF THE INVENTION

Implementations described herein relate generally to neural interfacing devices configured to electrically stimulate and/or record electrical activity of nerves.

Electrical stimulation can be employed for stimulating, inhibiting, or otherwise manipulating nerves, including peripheral nerves, cranial nerves, optic nerves, spinal nerves, autonomic nerves, nerve ganglia, plexuses of nerves, nervous tissue, and the like. The effects of electrical stimulation on a nerve and characteristics of neural recordings can be at least, partially controlled by the characteristics of the electrode used to contact the nerve. A major challenge in the art is minimizing the electrical current or voltage delivered by the electrode required to achieve the desired effect on the target nerve.

Existing approaches for interfacing nerves include interfaces that are affixed external to various tissue layers that typically surround nerves. Electrodes in these configurations are separated from target axons by one or more layers of tissue such as epineural tissue, connective tissues, fatty tissues, etc. that can be of high electrical impedance. In a stimulation setting, these tissues can require that more charge be delivered from the stimulating electrode to achieve the desired effect on target axons and in a recording setting obscure signals from target axons. Extraneural interfaces can also face challenges of migrating in space over time with respect to target axons.

Previous studies have shown that selective stimulation and/or recording capabilities are enhanced in interfascicular or intraneural interfaces, but these approaches are significantly invasive to the nerve. Additionally, their long-term efficacy and safety depend heavily upon the surgical technique used to implant them, and the electrodes are prone to damage from motion.

Accordingly, a need exists for improved neural interface and systems and methods thereof that are minimally invasive, reduce the required charge to be delivered to a nerve, increase the fidelity of recorded nerve activity, and provide stability to maintain the electrode position on the nerve.

SUMMARY

It is to be understood that this summary is not an extensive overview of the disclosure. This summary is exemplary and not restrictive, and it is intended to neither identify key or critical elements of the disclosure nor delineate the scope thereof. The sole purpose of this summary is to explain and exemplify certain concepts of the disclosure as an introduction to the following complete and extensive detailed description.

In one embodiment, the present disclosure provides for a neural interfacing device comprising a microneedle electrode. The microneedle electrode may have one or more microneedles. The one or more microneedles may be shaped and positioned such that when the neural interfacing device is applied to a nerve, the microneedle penetrates a nerve epineurium without any portion of the microneedle electrode penetrating any nerve axon beyond a depth of 500 micrometers.

In another aspect, the neural interfacing device can be configured in a bipolar assembly having two microneedle electrodes. In another aspect, the neural interfacing device can be configured in a tri-polar assembly having three microneedle electrodes. In a further aspect, the neural interfacing device can be configured in a multi-channel array that is selectively configurable via external electronics in electrical communication with the plurality of microneedle electrodes.

Additional features and advantages of exemplary implementations of the invention will be set forth in the description which follows, and in part will be obvious from the description, or may be learned by the practice of such exemplary implementations. The features and advantages of such implementations may be realized and obtained by means of the instruments and combinations particularly pointed out in the appended claims. These and other features will become more fully apparent from the following description and appended claims, or may be learned by the practice of such exemplary implementations as set forth hereinafter.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a perspective view and cross-sectional view of a schematic showing a neural interfacing device interfacing with a nerve,

FIG. 2 is a perspective view of a schematic showing a neural interfacing device having three microneedle electrodes connected to stimulating electronics.

FIG. 3 is a graphical comparison of the noise inherent to electrical stimulation of a nerve using standard electrodes versus microneedle electrodes.

FIG. 4 is a top-down view of microneedle electrodes having different types of microneedles.

FIG. 5 is an illustration of a potential fabrication method of a neural interfacing device.

FIG. 6 is a radial cross section of a sciatic nerve with a microneedle electrode implanted.

FIG. 7 shows three charts comparing the electrical performance of microneedle electrodes to conventional electrodes in an in-vivo setting.

FIG. 8 is a perspective view of a schematic showing a neural interfacing device having a 2x2 array of microneedle electrodes attached to a planar assembly.

FIG. 9 shows examples of commercial embodiments of planar neural interfacing assemblies.

DETAILED DESCRIPTION

The present invention can be understood more readily by reference to the following detailed description, examples, drawing, and claims, and their previous and following description. However, before the present devices, systems, and/or methods are disclosed and described, it is to be understood that this invention is not limited to the specific devices, systems, and/or methods disclosed unless otherwise specified, as such can, of course, vary. It is also to be understood that the terminology used herein is for the purpose of describing particular aspects only and is not intended to be limiting.

The following description of the invention is provided as an enabling teaching of the invention in its best, currently known aspect. To this end, those skilled in the relevant art will recognize and appreciate that many changes can be made to the various aspects of the invention described herein, while still obtaining the beneficial results described herein. It will also be apparent that some of the desired

benefits described herein can be obtained by selecting some of the features described herein without utilizing other features. Accordingly, those who work in the art will recognize that many modifications and adaptations to the present invention are possible and can even be desirable in certain circumstances and are a part described herein. Thus, the following description is provided as illustrative of the principles described herein and not in limitation thereof.

Reference will be made to the drawings to describe various aspects of one or more implementations of the invention. It is to be understood that the drawings are diagrammatic and schematic representations of one or more implementations, and are not limiting of the present disclosure. Moreover, while various drawings are provided at a scale that is considered functional for one or more implementations, the drawings are not necessarily drawn to scale for all contemplated implementations. The drawings thus represent an exemplary scale, but no inference should be drawn from the drawings as to any required scale.

In the following description, numerous specific details are set forth in order to provide a thorough understanding described herein. It will be obvious, however, to one skilled in the art that the present disclosure may be practiced without these specific details. In other instances, well known aspects of electrical nerve stimulation and microfabrication techniques have not been described in particular detail in order to avoid unnecessarily obscuring aspects of the disclosed implementations.

As used in the specification and the appended claims, the singular forms “a,” and “the” include plural referents unless the context clearly dictates otherwise. Ranges may be expressed herein as from “about” one particular value, and/or to “about” another particular value. When such a range is expressed, another aspect includes from the one particular value and/or to the other particular value. Similarly, when values are expressed as approximations, by use of the antecedent “about,” it will be understood that the particular value forms another aspect. It will be further understood that the endpoints of each of the ranges are significant both in relation to the other endpoint, and independently of the other endpoint.

“Optional” or “optionally” means that the subsequently described event or circumstance may or may not occur, and that the description includes instances where said event or circumstance occurs and instances where it does not.

Throughout the description and claims of this specification, the word “comprise” and variations of the word, such as “comprising” and “comprises,” means “including but not limited to,” and is not intended to exclude, for example, other additives, components, integers or steps. “Exemplary” means “an example of” and is not intended to convey an indication of a preferred or ideal aspect. “Such as” is not used in a restrictive sense, but for explanatory purposes.

Disclosed are components that can be used to perform the disclosed methods and systems. These and other components are disclosed herein, and it is understood that when combinations, subsets, interactions, groups, etc. of these components are disclosed that while specific reference of each various individual and collective combinations and permutation of these may not be explicitly disclosed, each is specifically contemplated and described herein, for all methods and systems. This applies to all aspects of this application including, but not limited to, steps in disclosed methods. Thus, if there are a variety of additional steps that can be predefined it is understood that each of these additional steps can be predefined with any specific aspect or combination of aspects of the disclosed methods.

Implementations described herein are directed toward devices, systems and methods for neural interfacing, for example and without limitation, neural interfacing devices having microneedle electrodes. In one or more aspects, the neural interfacing device described herein comprises an elongate cuff body having a right and a left distal portion that communicate to define a lumen having a substantially reclosable opening. At least one microneedle electrode is fixed on an interior surface of the lumen defined by the cuff body. The at least one microneedle electrode comprises an array of microneedles. In one implementation, the neural interfacing device comprises at least one microneedle electrode having surface functionalized with microneedles that maximizes stimulation or inhibition of activity in but minimizes the charge delivered to the target nerve.

Reference will now be made to the drawings to describe various aspects of one or more implementations of the invention. It is to be understood that the drawings are diagrammatic and schematic representations of one or more implementations, and are not limiting of the present disclosure. Moreover, while various drawings are provided at a scale that is considered functional for one or more implementations, the drawings are not necessarily drawn to scale for all contemplated implementations. The drawings thus represent an exemplary scale, but no inference should be drawn from the drawings as to any required scale.

In the following description, numerous specific details are set forth in order to provide a thorough understanding described herein. It will be obvious, however, to one skilled in the art that the present disclosure may be practiced without these specific details. In other instances, well-known aspects of electrical nerve stimulation and microfabrication techniques have not been described in particular detail in order to avoid unnecessarily obscuring aspects of the disclosed implementations.

FIG. 1 shows two views of an example embodiment of a neural interfacing device interfacing with a nerve. In this particular embodiment, the neural interfacing device has two microneedle electrodes **102**. However, in other embodiments the neural interfacing device may have one microneedle electrode **102**. In yet other embodiments, the neural interfacing device may have up to 100 microneedle electrodes **102** or more. Each microneedle electrode **102** may comprise at least one microneedle **104**. In the embodiment of FIG. 1, each microneedle electrode **102** comprises an array of microneedles **104**. In other embodiments, each microneedle electrode **102** may have between 1 up to about 1000 microneedles **104** or more. The microneedles **104** may be arranged in any pattern, including for example a three-dimensional array, grid pattern, or different pattern.

Microneedle electrodes **102** may be connected to one another and/or connected to other electronic devices via electrical connectors **106**. Electrical connectors **106** may include any means for transmitting electrical charge and/or data. For example, the electrical connectors **106** may comprise wires, PCB boards, and/or flexible PCB with stretchable traces. In other embodiments, some of the electrical connectors **106** may be omitted in favor of a wireless transmitting device.

In some embodiments, the neural interfacing device comprises a body portion upon which one or more microneedle electrodes **102** may be mounted. For example, the embodiment of FIG. 1 shows an elongate cuff **114** upon which the microneedle electrodes **102** are mounted. However, the present disclosure is not limited to the use of an elongate cuff. In other embodiments, the microneedle electrodes **102** are mounted to a surface of a planar base. In some embodi-

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ments, the type of nerve can influence the preferred body portion for mounting a microneedle electrode. For example, for stimulating a standalone nerve that has adequate access, an elongate cuff may be used to at least partially surround a portion of the nerve. On the other hand, stimulating a tightly packed bundle of nerves may be more efficiently accomplished using a planar base that contacts the bundle of nerves rather than surrounding the nerves. In other embodiments, either a planar base or an elongate cuff, or both, may be employed. In other embodiments the planar base and the microneedle may be formed monolithically utilizing a biocompatible polymer that can be metallized to define microneedle electrodes. Other types of body portions may be used to mount the microneedle electrodes as well.

In some embodiments, the neural interfacing device comprises an elongate cuff body having a right and a left distal portion that communicate to define a lumen having a substantially re-closable opening. The cuff body need not completely enclose a nerve. For example, it may only enclose a portion of the nerve while leaving a portion of the nerve undisturbed. In that sense the word "lumen" is not intended to necessarily require a fully enclosed cavity or area.

In FIG. 1, an elongate cuff **114** is shown for securing the microneedle electrodes **102** to a nerve. A space **112** is shown in between the elongate cuff **114** and the nerve. However, the space **112** need not be maintained. In practice there may be more or less space, or none at all.

In the embodiment of FIG. 1, the microneedles **104** penetrate the epineurium **110** layer of the nerve. A person of ordinary skill in the art would recognize that the microneedles **104** may also penetrate other tissue layers, such as connective tissue, peripheral tissue, and others, while also penetrating the epineurium **110**. Additionally, not all of the microneedles **104** must penetrate the epineurium **110**. In some embodiments, only one microneedle **104** can penetrate the epineurium **110**. When multiple microneedles **104** are employed, different microneedles **104** may penetrate to different depths with the epineurium **110** and may penetrate all the way through the epineurium **110**.

FIG. 1 illustrates a general axon area **108** in the center of the nerve. A person of ordinary skill in the art would recognize that nerves typically contain many axons. For ease of discussion, these many axons are described as the "axon area," "axons," or "axon," interchangeably. In the embodiment of FIG. 1, none of the microneedles **104** penetrate into the axon area **108**. In other embodiments, at least one microneedle **104** may penetrate the axon area **108** up to a depth that constitutes minimal invasion into the axons. For example, in some embodiments the microneedles **104** do not penetrate more than about 500 micrometers into the axon area **108** or, alternatively stated, do not penetrate more than about 500 micrometers into any particular axon of the nerve at issue. In other embodiments, the microneedles **104** do not penetrate more than about 400 micrometers. In another embodiment, the microneedles **104** do not penetrate more than about 300 micrometers. In a further embodiment, the microneedles **104** do not penetrate more than about 200 micrometers. In yet another embodiment, the microneedles **104** do not penetrate more than about 100 micrometers. Finally, in some embodiments, the microneedles **104** do not penetrate the axon area **108**, and/or any particular axon, at all.

FIG. 2 shows an embodiment of a neural interfacing device having three microneedle electrodes **102**. Each microneedle electrode **102** is connected to at least one electronics module **116**. The connection may be made via electrical connectors **106**. An expanded view of the elec-

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tronics module **116** is shown in FIG. 2 and labeled as **118**. The expanded view provides a few examples of what the electronics module **116** may include. For example, it may include stimulating electronics for stimulating nerves, recording electronics including filters, amplifiers, and/or analog-digital converter. It may also include a rechargeable battery. A wireless transmitter may also be included in order to transmit information to, for example, a computer or other electronic device. In some embodiments, the electronics module **116** itself may be a computer, smartphone, tablet, or other computing device.

The embodiment of FIG. 2 shows three microneedle electrodes **102**. As explained above, the neural interfacing device may comprise any number of microneedle electrodes **102**. In some embodiments, where more than one microneedle electrode **102** is used, at least one of the microneedle electrodes **102** is a stimulating electrode that provides an electrical stimulus to a nerve, while at least one of the remaining microneedle electrodes **102** is a reference electrode. When more than two microneedle electrodes **102** are used, any combination of stimulating electrodes and reference electrodes may be employed.

In one aspect, the nerve interfacing device can comprise two microneedle electrodes that form a bipolar electrode assembly. Here, the first microneedle electrode can be configured as a stimulation electrode and the second microneedle electrode can be configured as a reference or a ground electrode. In another aspect, the electrode assembly can comprise three electrodes that form a tri-polar electrode assembly. Here, in one aspect, the first and second microneedle electrodes communicate to form a reference electrode and the third electrode is configured as a stimulation electrode. In a further aspect, the microneedle electrodes can be configured in a multichannel array that is selectively configurable via stimulation electronics in electrical communication with the plurality of microneedle electrodes.

FIG. 3 provides an example graphical comparison of the raw signals obtained from a neural interface device using standard electrodes versus microneedle electrodes. Both graphs show raw data recording during upstream electrical stimulation of a rat sciatic nerve. Graph **312** depicts the recording of compound activity using a tri-polar design with standard "off the shelf" electrodes having no microneedles. Graph **310** depicts recording of the same activity using microneedle electrodes disclosed herein. From left to right, the initial signal deflections represent the electrical stimulation artifact. This artifact is followed by an "A fiber" or "fast component" response shown as the next large signal deflections. Enhanced signal-to-noise ratio is merely one advantage of the disclosed microneedle electrodes herein.

FIG. 4 shows a design drawing of two example embodiments of the present disclosure. In these embodiments, microneedle electrodes **410** are shown having an array of microneedles **412**. In one embodiment, the microneedles **412** are formed by removing material from portions of the microneedle electrodes **410** to create voids **414**. As a result of those voids **414**, a force may be applied to fold the microneedles **412** away from the body of the microneedle electrodes **410** such that the microneedles **412** extend outward in a three-dimensional fashion. As illustrated by these two embodiments, the size and shape of the microneedles **412** may vary according to the desired implementation.

FIG. 5 illustrates one example method of fabrication a microneedle electrode. In this embodiment, the first step involves forming a first layer of Kapton **510**. Next, metal pads **512** are defined on the Kapton **510** substrate using, for

example, established microfabrication processes such as thin film deposit/etch, thin film lift-off, screen printing, electroplating, electroless plating, shadow masking of thin film metal, and the like. Metal pads **512** may include additional components for interacting with microneedle electrodes. For example, they may include traces for electrical connections. Additionally, electrical connector **514** is attached to the Kapton **512** layer to support a wire **518** connecting to, for example, external electronics. Electrical connector **514** may take the form of any component capable of electrical communication, including wireless transmission. In this embodiment, the next step is placing microneedle electrodes **516** onto the metal pads **512**. Finally, a second layer of Kapton **510** is added. In some embodiments, the second layer of Kapton **510** covers at least a portion of the metal pads **512** and/or the microneedle electrodes **516**. This particular method of fabrication is merely one example; a person of ordinary skill would understand that any other suitable fabrication techniques may be utilized.

In another aspect, the microneedle arrays can be formed monolithically on the substrate by using polymer micromachining and micromolding technologies. In this implementation, the substrate can be a flexible or standard polymer such as, for example and without limitation, PDMS, thin Kapton, thin polyimide, thin polyethylene naphthalate, SU-8, PMMA (poly methyl methacrylate), COO (cyclic olefin copolymer), PLGA (polylactic-co-glycolic acid), PLA (polylactic acid), or other suitable substitutes. Further, it is contemplated that the packaging can comprise, for example and without limitation, flex circuit interfacing with the microneedle electrode through mechanical fusion or using conductive PDMS or conductive epoxies as an intermediate material.

The microneedles may be manufactured from various materials, including at least one of stainless steel, platinum, platinum/iridium, palladium, silver, silver chloride, titanium nitride, titanium, iridium, iridium oxide, iridium tin oxide, PEDOT, carbon nanotubes epoxies, polymers, and conductive polymers. Further, it is contemplated that the packaging can comprise, for example and without limitation, flex circuit interfacing with the microneedle electrode through mechanical fusion or using conductive PDMS or conductive epoxies as an intermediate material.

FIG. 6 shows a radial cross section of a sciatic nerve with a microneedle electrode **102** implanted. From this angle, five microneedles **104** of the microneedle electrode **102** are visible. All of the visible microneedles **104** appear to have penetrated at least a portion of the epineurium layer of the nerve. Some of those microneedles **104** also appear to have penetrated the axon area of the nerve, but only minimally. In some embodiments, this penetration is less than 500 micrometers. As explained above, in different embodiments the microneedles **104** may not penetrate the axon area at all, or may penetrate any distance from between about 0 to about 500 micrometers.

FIG. 7 highlights the advantages of using microneedles **104** as disclosed herein, especially with respect to using a planar electrode that merely interfaces with the outer surface of a nerve. As shown in the charts of FIG. 7, nerve-electrode impedance decreases as needle height increases up to, for example, 200 micrometers. Similarly, stimulation threshold decreases up to 200 micrometers. Finally, the signal-to-noise ratio increases up to 200 micrometers. In one aspect, the microneedle surface configuration can lower the amount of current required for stimulation compared to conventional electrodes, thereby increasing safety and increasing the lifetime of the microneedle electrodes when used in chronic

settings. In another aspect, the microneedle surface configuration can increase the signal-to-noise ratio of nerve recordings over conventional electrodes. These advantages may lead to longer battery life of implantable devices. Additionally, lower current requirements may prevent nerve damage over time. Finally, lower currents may also lead to longer electrode life due to less degradation of electrical characteristics.

FIG. 8 shows an embodiment of a neural interfacing device having a 2x2 array of microneedle electrodes **812** attached to a planar assembly **810**. As discussed above, a planar assembly **810** may be employed instead of, or in addition to, a cuff assembly. Other shapes and sizes of assemblies are contemplated. However, a planar assembly may be more suitable for applying microneedle electrodes **812** to bundles of nerves that may otherwise be difficult to access with a cuff assembly. The embodiment shown in FIG. 8 illustrates the microneedle electrodes **812** having microneedles **814** as well as wires **816** leading to, for example, external electronics.

FIG. 9 shows examples of commercial embodiments of neural interfacing devices. For example, the figure shows a neural interfacing device having a 2x2 array of microneedle electrodes **912** attached to a planar assembly **910**. FIG. 9 also shows an array of microneedles **914** protruding from the microneedle electrodes **912** in a three-dimensional fashion. A plurality of wires **916** are also shown protruding from a microneedle electrode. Other wire configurations, including having different numbers of wires, are also contemplated.

It is also contemplated that the microneedle surface can increase the mechanical stability of the electrode assembly and therefore the performance of the system by reducing or eliminating any relative movement between the at least one microneedle electrode and target nerve. For example, the penetration of microneedles into the epineurium may serve to act as an anchor for the neural interfacing device. In one embodiment, the anchoring effect of the microneedles causes the microneedle electrode to remain in one position on the nerve. This, in turn, provides the entire neural interfacing device with additional stability relative to the nerve. For example, the neural interfacing device is less likely to slide along a nerve or rotate about the nerve when the microneedles have penetrated the epineurium of the target nerve or bundle of nerves. Additionally, anchoring may help to maintain sufficient contact between the microneedle electrodes and the nerve, thus lowering the current requirements for stimulation.

In one operational aspect, after a target nerve is exposed, the neural interfacing device can be applied where the at least one microneedle electrode is in contact with a target location on the nerve, the cuff can be connected to stimulation electronics, and the stimulation electronics can cause stimulation of the nerve via the microneedle electrodes. During and immediately after stimulation, data can be collected from a point downstream from the target location either on the nerve or an associated muscle in order to establish the stimulation threshold required for maximum stimulation. Also, with the same configuration, a stimulus could be applied to a location on the nerve downstream from the target location and the response of the nerve recorded at the target location via the microneedle electrode in order to establish a signal-to-noise ratio. It is contemplated that the neural interfacing device can have a wired configuration where the microneedle electrode assembly and stimulation electronics are connected via wires.

In one embodiment, the neural interfacing device comprises at least one microneedle having a height of from about

10 micrometers to about 10 millimeters. In another aspect, the at least one microneedle can have a sharpness from about 0.1 to about 100 micrometers. In yet another aspect, the microneedle electrode can have a pitch separating it from the neighboring electrode of from about 100 micrometers to about 100 millimeters. The thickness of the material comprising the microneedles can be at least about 10 micrometers to about 2 millimeters. In another aspect, the microneedle electrode can have from one microneedle to about 1000 microneedles forming an array. More preferably, the microneedle electrode has from about two microneedles per array to about 100 microneedles per array.

In one embodiment, the neural interfacing device may include an electrical shielding layer on an outer surface of the device. For example, if the neural interfacing device includes an elongate cuff, the elongate cuff may have an electrical shielding layer on its outer surface. In some embodiments the electrical shielding layer functions to shield the electronic components from electrical noise, thereby strengthening the signals sent to and from the microneedle electrodes.

In a further or additional aspect, the nerve interfacing device of the present invention could be used to regenerate severed or otherwise damaged nerves. Here, it is contemplated that the microneedle surface can serve to bind a severed or damaged nerve, and the external stimulation of the nerve via the microneedle electrode can facilitate nerve repair or regeneration.

Accordingly, FIGS. 1-7 and the corresponding text provide a number of different components and mechanisms for electrical stimulation of or recording activity of nerves. In addition to the foregoing, implementations described herein can also be described in terms acts and steps in a method for accomplishing a particular result. For example, a method comprising at least one of exposing a nerve, placing at least one microneedle electrode comprising a microneedle array in contact with a target location on the nerve, securing the at least one microneedle electrode about the nerve, placing the microneedle electrode in communication with stimulating electronics, stimulating the nerve and recording the electrical activity of the nerve is described concurrently above with reference to the components and diagrams of FIGS. 1-7.

The present invention can thus be embodied in other specific forms without departing from its spirit or essential characteristics. The described aspects are to be considered in all respects only as illustrative and not restrictive. The scope of the invention is, therefore, indicated by the appended claims rather than by the foregoing description. All changes that come within the meaning and range of equivalency of the claims are to be embraced within their scope.

What is claimed is:

1. An extraneural interfacing device, comprising:

a microneedle electrode comprising a plurality of microneedles, wherein the microneedle electrode comprises a conductive base having a plurality of voids, wherein each void of the plurality of voids forms a zigzag shape surrounding at least one row of the plurality of microneedles, wherein the at least one row of microneedles is bent outward with respect to the conductive base to form a three-dimensional microneedle electrode;

wherein each of the plurality of microneedles is shaped and positioned such that when the extraneural interfacing device is applied to a nerve, each of the microneedles penetrates a nerve epineurium without any portion of the microneedle electrode penetrating any nerve axon beyond a depth of 500 micrometers,

and wherein the microneedle electrode is configured as a single channel for applying stimulus or receiving data.

2. The extraneural interfacing device of claim 1, further comprising: a planar base comprising an inner surface and an outer surface; and wherein the microneedle electrode is fixed to the inner surface of the planar base.

3. The extraneural interfacing device of claim 1, further comprising: an elongate cuff comprising an outer surface and an inner surface and sized to fit at least partially around the nerve; wherein the microneedle electrode is fixed to the inner surface of the elongate cuff; and wherein the elongate cuff is configured to fit to the nerve.

4. The extraneural interfacing device of claim 1, wherein each of the microneedles penetrates the nerve epineurium without any portion of the microneedle electrode penetrating any nerve axon.

5. The extraneural interfacing device of claim 1, wherein when the microneedle electrode is applied to a nerve or bundle of nerves, the microneedle electrode anchors the extraneural interfacing device with respect to the nerve or bundle of nerves.

6. The extraneural interfacing device of claim 5, wherein the microneedle electrode provides stability to the extraneural interfacing device such that it remains in position with respect to the nerve or bundle of nerves.

7. The extraneural interfacing device of claim 1, wherein each of the microneedles has a height of about 10 micrometers to about 10 millimeters.

8. The extraneural interfacing device of claim 1, wherein the conductive base is a metal pad.

9. The extraneural interfacing device of claim 1, wherein the microneedle electrode comprises between 2 and 1000 microneedles.

10. The extraneural interfacing device of claim 1, wherein the extraneural interfacing device comprises at least two microneedle electrodes.

11. The extraneural interfacing device of claim 1, wherein the extraneural interfacing device comprises at least three microneedle electrodes.

12. The extraneural interfacing device of claim 1, further comprising an array of microneedle electrodes.

13. The extraneural interfacing device of claim 12, wherein the array of microneedle electrodes is a grid pattern having from 4 to 1000 microneedle electrodes.

14. The extraneural interfacing device of claim 1, wherein the extraneural interfacing device is connected to stimulation electronics via electrical connectors.

15. The extraneural interfacing device of claim 1, wherein the microneedle electrode is a single electrode.

16. The extraneural interfacing device of claim 1, wherein each void of the plurality of voids forms the zigzag shape surrounding two rows of interdigitated microneedles.

17. A method of gathering information on nerve activity, comprising:

accessing a nerve or bundle of nerves;

placing a microneedle electrode comprising a plurality of microneedles in contact with a target location on the nerve or bundle of nerves such that each of the plurality of microneedles penetrates a nerve epineurium without any portion of the microneedle electrode penetrating any nerve axon beyond a depth of 500 micrometers;

placing the microneedle electrode in communication with stimulating electronics;

stimulating the nerve or bundle of nerves; and

recording the electrical activity of the nerve or bundle of nerves as a result of said stimulation, wherein the

microneedle electrode is configured as a single channel for applying stimulus or receiving data, wherein the microneedle electrode comprises a conductive base having a plurality of voids, wherein each void of the plurality of voids forms a zigzag shape surrounding the at least one row of the plurality of microneedles, and wherein the at least one row of the plurality of microneedles is bent outward with respect to the conductive base to form a three-dimensional.

18. The method of claim 17, further comprising mounting the microneedle electrode to a planar base before placing the microneedle electrode in contact with the target location.

19. The method of claim 17, further comprising mounting the microneedle electrode to an elongate cuff before placing the microneedle electrode in contact with the target location.

20. The method of claim 17, further comprising monitoring electrical signals within the nerve or bundle of nerves using the microneedle electrode.

21. The method of claim 17, further comprising applying an electrical stimulus to the nerve or bundle of nerves using the microneedle electrode.

22. The method of claim 17, wherein each void of the plurality of voids forms the zigzag shape surrounding two rows of interdigitated microneedles.

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